Elastohydrodynamics of a pre-stretched finite elastic sheet lubricated by a thin viscous film with application to microfluidic soft actuators

Evgeniy Boyko¹, Ran Eshel¹, Khaled Gommed¹, Amir D. Gat^{1,†} and Moran Bercovici^{1,2,†}

¹Faculty of Mechanical Engineering, Technion – Israel Institute of Technology, Haifa 3200003, Israel

²Department of Mechanical Engineering, The University of Texas at Austin, Austin, Texas, TX 78712, USA

(Received 1 January 2018; revised 26 November 2018; accepted 26 November 2018; first published online 14 January 2019)

The interaction of a thin viscous film with an elastic sheet results in coupling of pressure and deformation, which can be utilized as an actuation mechanism for surface deformations in a wide range of applications, including microfluidics, optics and soft robotics. Implementation of such configurations inherently takes place over finite domains and often requires some pre-stretching of the sheet. Under the assumptions of strong pre-stretching and small deformations of the lubricated elastic sheet, we use the linearized Reynolds and Föppl-von Kármán equations to derive closed-form analytical solutions describing the deformation in a finite domain due to external forces, accounting for both bending and tension effects. We provide a closed-form solution for the case of a square-shaped actuation region and present the effect of pre-stretching on the dynamics of the deformation. We further present the dependence of the deformation magnitude and time scale on the spatial wavenumber, as well as the transition between stretching- and bending-dominant regimes. We also demonstrate the effect of spatial discretization of the forcing (representing practical actuation elements) on the achievable resolution of the deformation. Extending the problem to an axisymmetric domain, we investigate the effects arising from nonlinearity of the Reynolds and Föppl-von Kármán equations and present the deformation behaviour as it becomes comparable to the initial film thickness and dependent on the induced tension. These results set the theoretical foundation for implementation of microfluidic soft actuators based on elastohydrodynanmics.

Key words: Hele-Shaw flows, MEMS/NEMS, Microfluidics

1. Introduction

Elastohydrodynamic interaction between an elastic substrate and a thin liquid film is of interest in the study of various natural processes, such as passage of air flow in the lungs (Grotberg & Jensen 2004) and geological formation of laccoliths (Michaut

†Email addresses for correspondence: amirgat@technion.ac.il, mberco@technion.ac.il

2011), as well as in the dynamic control of elastic structures for applications in soft robotics, adaptive optics and reconfigurable microfluidics (Thorsen, Maerkl & Quake 2002; Chronis *et al.* 2003; Kim, Laschi & Trimmer 2013). In particular, the case of a viscous fluid confined between an elastic sheet and a rigid surface has been extensively studied in the context of viscous peeling (Hosoi & Mahadevan 2004; Lister, Peng & Neufeld 2013; Hewitt, Balmforth & De Bruyn 2015), suppression of viscous fingering instabilities (Pihler-Puzović *et al.* 2012, 2013; Al-Housseiny, Christov & Stone 2013; Pihler-Puzović, Juel & Heil 2014), impact mitigation (Tulchinsky & Gat 2016), elastohydrodynamic wakes (Arutkin *et al.* 2017) and dynamics of wrinkling of a lubricated elastic sheet (Kodio, Griffiths & Vella 2017).

In the field of microfluidics, where channels are often fabricated from soft materials such as poly(dimethylsiloxane) (PDMS), there is growing interest in exploring the effect of elasticity on the resulting flow and pressure fields, and several theoretical works have addressed this subject (Gervais et al. 2006; Dendukuri et al. 2007; Hardy et al. 2009; Panda et al. 2009; Mukherjee, Chakraborty & Chakraborty 2013; Christov et al. 2018). For example, Gervais et al. (2006) used a one-dimensional model, based on the assumption of a linear relation between fluidic pressure and channel deformation, to estimate the effect of elasticity on the pressure field in a shallow elastic micro-channel, showing good agreement with their experimental results. Recently, Christov et al. (2018) applied the lubrication approximation and the Kirchhoff-Love bending model to derive the relation between flow rate and pressure drop for a deformable shallow micro-channel. In tandem with the effect of elasticity on the flow field, the use of fluidic forces as an actuation mechanism for deformation of elastic substrates has also been exploited in a variety of applications, primarily as an on-chip valving method (Unger et al. 2000; Grover et al. 2006), and recently also for other applications including adaptive optics (Jeong et al. 2004) and soft robotics (Shepherd et al. 2011).

Of particular interest are soft planar microfluidic configurations, which may serve as a platform for re-configurable microstructures. For such configurations, thin elastic sheets (e.g. a $\sim 10 \ \mu m$ polymer sheet) are a natural choice for maximizing deformations. While tension reduces elastic deformations, it is difficult to implement robust set-ups without introducing some pre-stretching of the sheets. Thus, pure bending models (e.g. such as the one considered by Rubin et al. (2017) in previous work from our group) are insufficient for describing the behaviour of realistic systems. Furthermore, accurate prediction of the deformation field requires accounting for the influence of the finite boundaries of the sheet. As an example, and to relate the theoretical model studied in this work to realistic configurations, figure l(a,b)presents an experimental set-up in which a thin elastic membrane, pre-stretched on a rigid frame, serves as the ceiling of a Hele-Shaw chamber. The elastic sheet is actuated by an internal pressure gradient formed by opposing electro-osmotic flows (EOF) within the chamber. Additional details are provided in appendix A of the supplementary material is available online at https://doi.org/10.1017/jfm.2018.967. Figure 1(c) presents experimental results showing that indeed EOF-based deformations are feasible in practice. We note that, since the presented measurements are focused on a single point, the observed over-damped response can be easily fitted with various sets of realistic physical parameters and thus cannot be used for proper validation of the model. Such validation would require an imaging system which would allow much faster data acquisition as well as imaging of complete surfaces rather than an individual point. We are currently developing this infrastructure, which will be reported in the future.

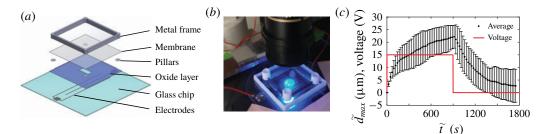


FIGURE 1. (Colour online) (a) Illustration and (b) image of an experimental set-up for deformation of an elastic sheet, actuated by non-uniform electro-osmotic flow. The configuration consists of a 12 μ m thick low-density polyethylene sheet stretched over a rigid frame that is supported by 100 μ m tall pillars from a rigid glass substrate, forming a Hele-Shaw chamber. The glass surface is patterned with three parallel electrodes and coated with an insulating oxide layer, excluding a rectangular actuation region at the centre. The chamber is filled with an aqueous solution, and the voltage is set to drive electro-osmotic flow from the outer electrodes to the inner ones, resulting in internal pressure gradients. (c) Experimental results showing the growth and decay of deformation at the centre of the elastic membrane, in response to sudden actuation and cessation of the electric field. Error bars indicate a 95% confidence on the mean based on six repeats, and the red curve represents the corresponding applied voltage as a function of time.

In this work, we aim to set the theoretical framework for addressing such configurations, where finite boundaries, pre-stretching and fluidic actuation dominate the physical response of the system. In $\S 2$, we present the problem formulation and the equations governing the deformation dynamics, accounting for both bending and stretching, as well as for forces applied either through the non-uniform slip velocity in the fluid or due to the pressure applied directly to the elastic sheet. We provide their scaling and summarize the key assumptions used in the derivation of the model. Focusing on electro-osmotic actuation, in $\S 3$ we present a closed-form solution for the practical case of a square-shaped actuation region within a finite rectangular domain. We present the effect of pre-stretching on the steady-state deformation pattern and magnitude, and examine the time scales for development of pressure and deformation. Using a Fourier decomposition, in §4 we further study the trade-off between the amplitude and time scale of deformations and the attainable spatial resolution, and show their different scaling in tension- versus bending-dominant regimes. In §5, we examine the effect of spatial discretization of the forcing (representing, e.g. actuation electrodes) on the resulting deformation, minimizing the error between the resulting and desired deformation using a least-squares method. Considering an axisymmetric domain, in §6 we employ asymptotic and numerical methods to explore the effects arising from nonlinearity of the Reynolds and Föppl-von Kármán equations, and further examine the influence of these effects on the deformation and tension field. We conclude with a discussion of the results in $\S7$.

2. Problem formulation and governing equations

We study the viscous-elastic dynamics of a viscous fluid of density $\tilde{\rho}$ and viscosity $\tilde{\mu}$ confined between a flat rigid surface and a pre-stretched elastic sheet of length \tilde{l}_m , width \tilde{w}_m , thickness \tilde{h}_m , Young's modulus \tilde{E}_Y and Poisson's ratio ν , as shown in figure 2. We denote dimensional variables by tildes, normalized variables without

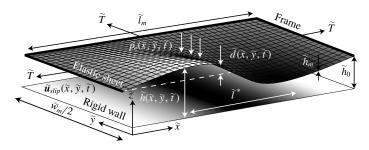


FIGURE 2. Schematic illustration showing the centreline cross-section of the examined configuration. A thin viscous fluid layer of initial thickness \tilde{h}_0 is confined between a rigid surface and a pre-stretched elastic sheet supported at its boundaries. Non-uniform and time-varying slip velocity $\tilde{u}_{slip}(\tilde{x}, \tilde{y}, \tilde{t})$ and external pressure $\tilde{p}_e(\tilde{x}, \tilde{y}, \tilde{t})$ drive the viscous–elastic interaction and create the deformation field $\tilde{d}(\tilde{x}, \tilde{y}, \tilde{t})$.

tildes and characteristic values by an asterisk superscript. We employ a Cartesian coordinate system $(\tilde{x}, \tilde{y}, \tilde{z})$, and adopt the \parallel and \perp subscripts to denote parallel and perpendicular directions to the $\tilde{x} - \tilde{y}$ plane, respectively.

The fluid velocity is $\tilde{\boldsymbol{u}} = (\tilde{\boldsymbol{u}}_{\parallel}, \tilde{\boldsymbol{u}}_{\perp}) = (\tilde{\boldsymbol{u}}, \tilde{\boldsymbol{v}}, \tilde{\boldsymbol{w}})$ and fluid pressure is \tilde{p} . The total gap between the plates is $\tilde{h}(\tilde{x}, \tilde{y}, \tilde{t}) = \tilde{h}_0 + \tilde{d}(\tilde{x}, \tilde{y}, \tilde{t})$, where \tilde{t} is time and \tilde{h}_0 is the initial gap. The deformation field $\tilde{d}(\tilde{x}, \tilde{y}, \tilde{t})$ is induced either due to an external pressure $\tilde{p}_e(\tilde{x}, \tilde{y}, \tilde{t})$, acting directly on the elastic sheet, or due to an internal pressure formed by a non-uniform slip velocity $\tilde{\boldsymbol{u}}_{slip}(\tilde{x}, \tilde{y}, \tilde{t})$ on the rigid surface, which varies over a characteristic length scale \tilde{l}^* in the $\tilde{x} - \tilde{y}$ plane. The characteristic velocities in the $\tilde{x} - \tilde{y}$ plane and \hat{z} direction are respectively \tilde{u}^* and \tilde{w}^* , and the characteristic pressure, deformation and time are respectively denoted as \tilde{p}^* , \tilde{d}^* , and \tilde{t}^* .

The most general description for the dynamics of a thin elastic sheet is given by the nonlinear Föppl-von Kármán equations (Timoshenko & Woinkowsky-Krieger 1987; Howell, Kozyreff & Ockendon 2009), which account for bending and tension forces, external traction, as well as the solid's inertia. In this work, we assume that the solid's inertia is negligible and focus on the case of a strongly pre-stretched elastic sheet with isotropic tension \tilde{T} , assumed to be much larger than any internal tension, \tilde{T}_{in} , forming in the system during actuation of the sheet. From scaling of the Föppl-von Kármán equation that couples the spatial variations in internal tension to Gaussian curvature (Howell *et al.* 2009, p. 176), we find $\tilde{T}_{in} \sim (\tilde{d}^*/\tilde{l}^*)^2 \tilde{E}_Y \tilde{h}_m$, and define

$$\alpha = \frac{\tilde{T}_{in}}{\tilde{T}} = \left(\frac{\tilde{d}^*}{\tilde{l}^*}\right)^2 \frac{\tilde{E}_Y \tilde{h}_m}{\tilde{T}} \ll 1.$$
(2.1)

Expanding the deformation field and the tension in powers of α and considering the leading order, the nonlinear Föppl–von Kármán equations reduce to a single linear plate equation containing bending and pre-stretching terms (see Timoshenko & Woinkowsky-Krieger 1987; Howell *et al.* 2009)

$$\tilde{p} = \tilde{B}\tilde{\nabla}_{\parallel}^{4}\tilde{d} - \tilde{T}\tilde{\nabla}_{\parallel}^{2}\tilde{d} + \tilde{p}_{e}, \qquad (2.2)$$

where $\tilde{\nabla}_{\parallel} = (\partial/\partial \tilde{x}, \partial/\partial \tilde{y})$ is the two-dimensional gradient and $\tilde{B} = \tilde{E}_Y \tilde{h}_m^3 / 12(1 - \nu^2)$ is the bending stiffness.

We restrict our analysis to shallow geometries, to negligible fluidic inertia, represented by small Womersley and reduced Reynolds numbers, and to small elastic deformations,

$$\epsilon = \frac{\tilde{h}_0}{\tilde{l}^*} \ll 1, \quad Wo = \frac{\tilde{\rho}\tilde{h}_0^2}{\tilde{\mu}\tilde{t}^*} \ll 1, \quad \epsilon Re = \epsilon \frac{\tilde{\rho}\tilde{u}^*\tilde{h}_0}{\tilde{\mu}} \ll 1, \quad \beta = \frac{\tilde{d}^*}{\tilde{h}_0} \ll 1. \quad (2.3a-d)$$

The first three assumptions (2.3a-c) allow us to apply the lubrication approximation and to obtain a nonlinear Reynolds equation (Leal 2007), and the last assumption, $\beta \ll 1$, enables its linearization (see e.g. Tulchinsky & Gat 2016; Kodio *et al.* 2017). In §6 we relax the assumptions (2.1) and (2.3d), and explore the effects of

nonlinearity of the Reynolds and Föppl-von Kármán equations on the deformation and tension fields, considering an axisymmetric geometry.

Based on (2.3), the fluid motion is governed by the lubrication equations (Leal 2007)

$$\tilde{\boldsymbol{\nabla}} \cdot \tilde{\boldsymbol{u}} = 0, \quad \tilde{\boldsymbol{\nabla}}_{\parallel} \tilde{p} = \tilde{\mu} \frac{\partial^2 \tilde{\boldsymbol{u}}_{\parallel}}{\partial \tilde{z}^2}, \quad \frac{\partial \tilde{p}}{\partial \tilde{z}} = 0.$$
(2.4*a*-*c*)

We assume that the fluid is subject to the slip and the no-penetration boundary conditions on the bottom surface. Horizontal motion of the elastic sheet is negligible in the small-deformation limit, implying the no-slip and the no-penetration boundary conditions along it,

$$(\tilde{\boldsymbol{u}}_{\parallel}, \tilde{\boldsymbol{u}}_{\perp})|_{\tilde{z}=0} = (\tilde{\boldsymbol{u}}_{slip}(\tilde{x}, \tilde{y}, \tilde{t}), 0), \quad (\tilde{\boldsymbol{u}}_{\parallel}, \tilde{\boldsymbol{u}}_{\perp})|_{\tilde{z}=\tilde{h}} = \left(\boldsymbol{0}, \frac{\partial \tilde{d}}{\partial \tilde{t}}\right).$$
(2.5*a*,*b*)

In this work, we consider a non-uniform slip velocity and specifically focus on the electro-osmotic slip which arises over electrically charged surfaces due to interaction of an externally applied electric field with the excess of net charge in the electric double layer. In the thin-double-layer limit, such interaction results in bulk fluid motion outside the outer edge of the electric double layer according to the Helmholtz–Smoluchowski equation (Hunter 2000),

$$\tilde{\boldsymbol{u}}_{slip} = -\frac{\tilde{\varepsilon}\zeta(\tilde{\boldsymbol{x}}, \tilde{\boldsymbol{y}})}{\tilde{\mu}}\tilde{\boldsymbol{E}},\tag{2.6}$$

where $\tilde{\varepsilon}$ is the fluid permittivity, $\tilde{\zeta}$ is the zeta potential on the bottom surface and \tilde{E} is the tangential imposed electric field.

2.1. Scaling analysis and non-dimensionalization

Scaling by the characteristic dimensions, we define the following normalized quantities: $(x, y, z) = (\tilde{x}/\tilde{l}^*, \tilde{y}/\tilde{l}^*, \tilde{z}/\tilde{h}_0)$, $(u, v, w) = (\tilde{u}/\tilde{u}^*, \tilde{v}/\tilde{u}^*, \tilde{w}/\tilde{w}^*)$, $p = \tilde{p}/\tilde{p}^*$, $t = \tilde{t}/\tilde{t}^*$, $d = \tilde{d}/\tilde{d}^*$ and $h = \tilde{h}/\tilde{h}_0$. As noted by Peng *et al.* (2015), the bending-tension length scale $\tilde{l}_{BT} = \sqrt{\tilde{B}/\tilde{T}}$ determines the relative importance of bending and tension forces in the elastic response of the sheet; for $\tilde{l}^* \ll \tilde{l}_{BT}$ bending forces dominate, whereas for $\tilde{l}^* \gg \tilde{l}_{BT}$ tension forces dominate. A convenient dimensionless number when scaling (2.2) is λ , defined as

$$\lambda \equiv \frac{\text{Bending}}{\text{Stretching}} = \left(\frac{\tilde{l}_{BT}}{\tilde{l}^*}\right)^2 = \frac{\tilde{B}}{\tilde{T}\tilde{l}^{*2}} = \frac{1}{12(1-\nu^2)} \frac{\tilde{E}_Y \tilde{h}_m}{\tilde{T}} \left(\frac{\tilde{h}_m}{\tilde{l}^*}\right)^2.$$
(2.7)

In this study, our main focus is on deformations which are comparable to, or larger than the sheet thickness, and therefore the appropriate scaling for deformation is based on tension and not on bending

$$\tilde{d}^* = \frac{\tilde{p}^* \tilde{l}^{*2}}{\tilde{T}},\tag{2.8}$$

with which the elastic equation (2.2) takes the form

$$p = \lambda \nabla_{\parallel}^4 d - \nabla_{\parallel}^2 d + p_e.$$
(2.9)

From order-of-magnitude analysis of the continuity and in-plane momentum equations (2.4*a*,*b*), it follows that the perpendicular velocity and the pressure scale as $\tilde{w}^* \sim \epsilon \tilde{u}^*$ and $\tilde{p}^* \sim 12\tilde{\mu}\tilde{u}^*/\epsilon^2\tilde{l}^*$, respectively. Using the kinematic boundary condition (2.5*b*) we obtain the scaling for the viscous–elastic time scale $\tilde{t}^* \sim \tilde{d}^*/\tilde{w}^* \sim \tilde{d}^*/\epsilon \tilde{u}^*$. Owing to a linear relation between \tilde{d}^* and \tilde{p}^* as well as between \tilde{p}^* and \tilde{u}^* , the ratio \tilde{d}^*/\tilde{u}^* is not dependent on actuation force, nor on \tilde{u}_{slip} or \tilde{p}_e . Thus, the viscous–elastic time scale solely depends on the properties of the fluid and the elastic medium, specifically the ratio $\tilde{\mu}/\tilde{T}$ and the geometry:

$$\tilde{t}^* = \frac{12\tilde{\mu}\tilde{l}^{*4}}{\tilde{T}\tilde{h}_0^3} = \frac{12\tilde{\mu}\tilde{l}^*}{\epsilon^3\tilde{T}}.$$
(2.10)

Based on this scaling, and following standard lubrication theory, from (2.4), (2.5) and (2.10) we obtain the normalized Reynolds equation (Leal 2007, p. 313)

$$\frac{\partial d}{\partial t} - \nabla_{\parallel} \cdot [h^3 \nabla_{\parallel} p] = -\frac{1}{2} \nabla_{\parallel} \cdot [h \boldsymbol{u}_{slip}], \qquad (2.11)$$

where using the definition (2.3*d*), the fluid thickness *h* can be expressed as $h = 1 + \beta d$.

2.2. Viscous–elastic governing equations for a pre-stretched elastic sheet Substituting (2.9) into (2.11), yields the nonlinear governing equation

$$\frac{\partial d}{\partial t} - \nabla_{\parallel} \cdot [h^3 \nabla_{\parallel} (\lambda \nabla_{\parallel}^4 d - \nabla_{\parallel}^2 d)] = -\nabla_{\parallel} \cdot [hf_F] + \nabla_{\parallel} \cdot [h^3 \nabla_{\parallel} f_E], \qquad (2.12)$$

where we define $f_F = f_{Fx}\hat{x} + f_{Fy}\hat{y} = u_{slip}/2$ and $f_E = p_e$ as the actuation mechanisms. The subscript *F* refers to driving force applied to the sheet due to the non-uniform slip velocity in the fluid and the subscript *E* refers to driving force due to the pressure applied directly to the elastic sheet.

Assuming small elastic deformations, $\tilde{d}^* \ll \tilde{h}_0$, yields the linearized viscous–elastic governing equation in terms of deformation accounting for both bending and pre-stretching (Kodio *et al.* 2017), which contains a source term that depends on the external forces

$$\frac{\partial d}{\partial t} - \lambda \nabla_{\parallel}^{6} d + \nabla_{\parallel}^{4} d = -\nabla_{\parallel} \cdot \boldsymbol{f}_{F} + \nabla_{\parallel}^{2} \boldsymbol{f}_{E}.$$
(2.13)

For completeness, the corresponding dimensional equation is given by

$$\frac{\partial d}{\partial \tilde{t}} - \frac{h_0^3}{12\tilde{\mu}} \tilde{\boldsymbol{\nabla}}_{\parallel} \cdot [\tilde{\boldsymbol{\nabla}}_{\parallel} (\tilde{B} \tilde{\boldsymbol{\nabla}}_{\parallel}^4 \tilde{d} - \tilde{T} \tilde{\boldsymbol{\nabla}}_{\parallel}^2 \tilde{d})] = -\tilde{h}_0 \tilde{\boldsymbol{\nabla}}_{\parallel} \cdot \tilde{\boldsymbol{f}}_F + \frac{h_0^3}{12\tilde{\mu}} \tilde{\boldsymbol{\nabla}}_{\parallel}^2 \tilde{f}_E.$$
(2.14)

. .

The governing equations (2.12)–(2.14) are supplemented by the boundary conditions

$$d = 0, \quad \frac{\partial^2 d}{\partial x^2} = 0, \quad \frac{\partial^4 d}{\partial x^4} = 0 \quad \text{at } x = 0, \, l_m \text{ and } 0 \le y \le w_m, \qquad (2.15a - c)$$

$$d = 0, \quad \frac{\partial^2 d}{\partial y^2} = 0, \quad \frac{\partial^4 d}{\partial y^4} = 0 \quad \text{at } y = 0, w_m \text{ and } 0 \le x \le l_m, \qquad (2.16a - c)$$

and the initial condition d(x, y, t=0) = 0. The first two boundary conditions (2.15a,b)and (2.16a,b) correspond to no deflection and no moment at the boundaries, whereas the last conditions (2.15c) and (2.16c) are obtained from (2.2) by further assuming that the fluidic and external pressures are both zero at the boundaries, $p = p_e = 0$ (see, e.g. Kodio *et al.* 2017). We note that the condition p = 0 is motivated by the experimental set-up shown in figure 1, where the fabricated chamber has open boundaries, which are well represented by zero gauge pressure. In addition, for the case of a tensiondominant regime, which is the main focus of this work, setting $\lambda = 0$ in (2.12)-(2.14) yields fourth-order governing equations. The boundary conditions (2.15a,b) and (2.16a,b) hold for this case, with the second derivative requirement arising directly from the zero pressure condition (rather than from the no-moment requirement in the sixth-order case).

The governing equation (2.13) can be solved by several methods. For the boundary conditions under consideration (2.15)–(2.16), eigenfunction expansions or a Green's functions approach are particularly suitable. We refer the reader to Prosperetti (2011) for both methods of solution, and note that in practice these calculations may be cumbersome. The general solution based on a Green's function approach for the case presented here is provided in appendix B of the supplementary material. However, we stress that both eigenfunctions and Green's functions approaches would be far more complex to implement if boundary conditions other than those presented here are adopted. Furthermore, analytical treatment would be greatly complicated, if at all possible, in non-rectangular and non-circular domains of interest.

3. Deformations due to a square-shaped actuation region

We now consider the non-uniform slip velocity (2.6) as a driving force and specifically focus on a square-shaped actuation of the form

$$f_{F_x}(x, y, t) = \begin{cases} E(t) & |x - c_x| \leq L \text{ and } |y - c_y| \leq L \\ 0 & \text{otherwise,} \end{cases}$$
(3.1)

corresponding to a square-shaped zeta-potential distribution, where E(t) is a spatially homogeneous and time-dependent electric field along the \hat{x} axis. Here 2L is the side length of the actuation square, whereas c_x and c_y indicate the x- and y-coordinates of its centre. For convenience, hereafter we set $l_m = w_m = \pi$.

For a suddenly applied actuation, E(t) = H(t), where H is the Heaviside step function, using closed-form solutions derived in appendix B of the supplementary material, we obtain the deformation field resulting from (3.1)

$$d(x, y, t) = \frac{16}{\pi^2} \sum_{m,n=1}^{\infty} \mathcal{A}(m, n; L, c_x, c_y) \frac{\sin(mx)\sin(ny)}{nF(m, n; \lambda)} (1 - e^{-F(m, n; \lambda)t}), \qquad (3.2a)$$

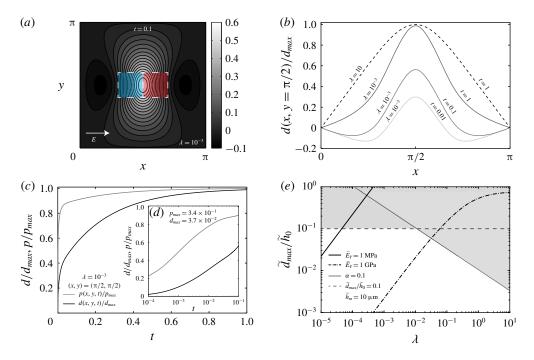


FIGURE 3. (Colour online) Investigation of the deformation field resulting from two square-shaped regions with opposite signs of zeta potential subjected to a constant electric field suddenly applied at t = 0. (a) The deformation field (colour map) at t = 0.1, superposed on a schematic illustration of the two oppositely directed electro-osmotic actuation regions. (b) The scaled steady-state deformation d/d_{max} along the \hat{x} axis, showing the evolution of the deformation for $\lambda = 10^{-3}$, and a comparison between the steady-state deformation at $\lambda = 10^{-3}$ (tension dominant, with $d_{max} = 3.7 \times 10^{-2}$) and $\lambda = 10$ (bending dominant, with $d_{max} = 1.2 \times 10^{-3}$). (c,d) The evolution of the maximum deformation and pressure as a function of time. (e) The maximum deformation \tilde{d}_{max} at steady state, scaled by \tilde{h}_0 , as a function of λ , for $\tilde{E}_Y = 1$ MPa and $\tilde{E}_Y = 1$ GPa. The dashed and solid grey lines indicate the validity boundaries $\tilde{d}_{max}/\tilde{h}_0 = 0.1$ and $\alpha = 0.1$, respectively, where the greyed-out region is beyond the validity of the model. All calculations were performed using $\tilde{l}^* = 5$ mm, $\tilde{h}_0 = 100 \ \mu$ m, $\tilde{p}^* \approx 1$ Pa, $\tilde{h}_m = 10 \ \mu$ m, $\nu = 0.5$, $c_{x,1} = 2\pi/5$, $c_{x,2} = 3\pi/5$, $c_{y,1} = c_{y,2} = \pi/2$ and $L = \pi/10$.

$$\mathcal{A} = \cos(mc_x)\sin(nc_y)\sin(mL)\sin(nL), \quad F = (m^2 + n^2)^2[\lambda(m^2 + n^2) + 1]. \quad (3.2b,c)$$

In appendix C of the supplementary material, we use numerical computations to verify the analytical solution (3.2) for the case of $\lambda = 0$, showing excellent agreement.

Figure 3(*a*) presents the deformation field (3.2) at t = 0.1, resulting from two square-shaped regions with opposite signs of zeta potential, subjected to an electric field suddenly applied at t=0 (see also supplementary movie 1). The opposing flows result in a positive internal pressure at the interface between the two regions, and negative pressure at the far edges of the squares. Figure 3(*b*) presents the deformation field (along the \hat{x} axis) as a function of time, for a pre-stretching-dominant regime $\lambda = 10^{-3}$. The steady-state deformation (t = 1) with $d_{max} = 3.7 \times 10^{-2}$ is compared with that obtained for a bending-dominant regime $(\lambda = 10)$ having $d_{max} = 1.2 \times 10^{-3}$,

showing that the higher order of the dominant term in the bending regime effectively results in additional averaging of the fluidic pressure and thus reduces the spatial resolution and the magnitude of the deformation field. Figure 3(c,d) presents the development of the maximum pressure and deformation as a function of time towards steady state, where $p_{max} = 3.4 \times 10^{-1}$ and $d_{max} = 3.7 \times 10^{-2}$. Importantly, while for a rigid configuration actuation of the electric field would result in an instantaneous jump in pressure (on an acoustic time scale), in the elastic case the evolution of the pressure is coupled to that of the deformation, as given by (2.11). Nevertheless, for the case presented, the rise time to 50% of the final pressure is $t = 10^{-3}$, nearly two orders of magnitude shorter than the viscous-elastic time scale $t = 0.7 \times 10^{-1}$ in which the deformation reaches 50% of its steady-state value. This time delay between pressure and deformation is also evident in periodic actuations (see supplementary movie 2) where the deformation phase lags behind that of the pressure. We note that at extremely short time scales, inertial effects must be included to properly describe the deformation dynamics. Figure 3(e) presents the maximum deformation (scaled by \tilde{h}_0) at steady state as a function of λ , for a fixed sheet thickness and two different elastic moduli. Consistent with the scaling (2.8) and non-dimensional solution (3.2), as λ increases (\tilde{T} decreases), the magnitude of the deformation increases until it reaches a constant value when the problem is dominated entirely by bending. The dashed and solid grey lines respectively indicate the range of validity of the model, where the deformation is no longer small, $\tilde{d}_{max}/\tilde{h}_0 = 0.1$, and where internal stretching is non-negligible, $\alpha = 0.1$. For clarity, the regions of the graph which are beyond the validity of the model are greyed out.

4. Effect of pre-stretching on the resolution, magnitude and time scale of the deformation field

As we are aiming to utilize fluidic actuation as a mechanism to create desired deformation in the elastic sheet, it is of interest to examine the trade-off between the magnitude and time scale of deformation's and the attainable resolution, for a given amplitude of the actuation force. Any desired deformation can be written as a Fourier series on a finite domain, where the resulting spectrum of frequencies would depend on the desired shape and on the deformation's position relative to the boundaries. Consider a steady-state deformation of the form

$$\tilde{d}(\tilde{x}, \tilde{y}) = \tilde{d}_0 \sin\left(k_x \pi \frac{\tilde{x}}{\tilde{l}_m}\right) \sin\left(k_y \pi \frac{\tilde{y}}{\tilde{w}_m}\right), \qquad (4.1)$$

created due to a non-uniform Helmholtz–Smoluchowski slip velocity, (2.6), acting in the \hat{x} direction. Here k_x and k_y are wavenumbers in the \hat{x} and \hat{y} directions, respectively, and \tilde{d}_0 is the amplitude yet to be determined. Using (2.6) and (2.14), the zeta potential required for generating the deformation (4.1) is given by

$$\tilde{\zeta}(\tilde{x},\tilde{y}) = \frac{\tilde{h}_0^2}{6\tilde{\varepsilon}\tilde{E}} \int (-\tilde{B}\tilde{\nabla}_{\parallel}^6\tilde{d} + \tilde{T}\tilde{\nabla}_{\parallel}^4\tilde{d}) \,\mathrm{d}\tilde{x} = \tilde{\zeta}_0 \cos\left(k_x\pi\frac{\tilde{x}}{\tilde{l}_m}\right) \sin\left(k_y\pi\frac{\tilde{y}}{\tilde{w}_m}\right), \quad (4.2)$$

enabling us to explicitly express the amplitude \tilde{d}_0 in terms of relevant physical quantities,

$$\tilde{d}_0 = -\frac{\tilde{6\varepsilon}\tilde{\zeta}_0\tilde{E}}{\pi^3\tilde{h}_0^2} \frac{k_x/\tilde{l}_m}{((k_x/\tilde{l}_m)^2 + (k_y/\tilde{w}_m)^2)^2(\pi^2\tilde{B}[(k_x/\tilde{l}_m)^2 + (k_y/\tilde{w}_m)^2] + \tilde{T})}.$$
(4.3)

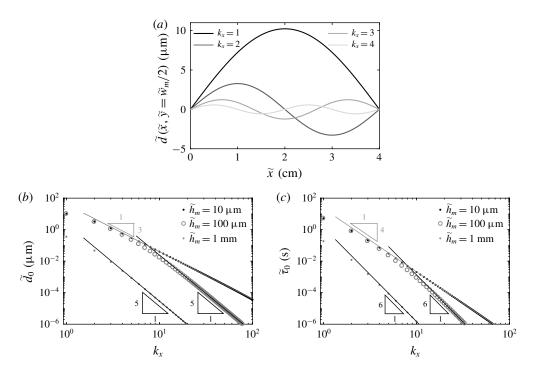


FIGURE 4. The effect of wavenumber on the magnitude of the deformation and the time scale of viscous–elastic interaction. (a) Deformation in dimensional form along the \hat{x} axis for various values of k_x , with $k_y = 1$ and $\tilde{h}_m = 10 \ \mu\text{m}$. (b,c) The maximum (dimensional) deformation \tilde{d}_0 and time scale $\tilde{\tau}_0$, respectively, as a function of wavenumber k_x , for $k_y = 1$ and different values of the elastic sheet thickness, \tilde{h}_m . All calculations were performed using non-uniform electro-osmotic actuation as the driving mechanism, with $\tilde{h}_0 = 100 \ \mu\text{m}$, $\tilde{l}_m = \tilde{w}_m = 4 \ \text{cm}$, $\tilde{E}_y = 0.3 \ \text{GPa}$, $\nu = 0.5$, $\tilde{T} = 15 \ \text{Pa} \ \text{m}$, $\tilde{\zeta}_0 = -70 \ \text{mV}$, $\tilde{E} = 100 \ \text{V} \ \text{cm}^{-1}$ and $\tilde{\varepsilon} = 7.08 \times 10^{-10} \ \text{F} \ \text{m}^{-1}$.

Substituting (4.2) into (2.14), we obtain the corresponding time-dependent solution

$$\tilde{d}(\tilde{x}, \tilde{y}, \tilde{t}) = \tilde{d}_0 \sin\left(k_x \pi \frac{\tilde{x}}{\tilde{l}_m}\right) \sin\left(k_y \pi \frac{\tilde{y}}{\tilde{w}_m}\right) (1 - e^{-\tilde{t}/\tilde{\tau}_0}),$$
(4.4)

that evolves towards steady-state deformation $\tilde{d}(\tilde{x}, \tilde{y})$, (4.1), and provides the viscouselastic time scale $\tilde{\tau}_0$ required to achieve this steady state,

$$\tilde{\tau}_0 = \frac{12\tilde{\mu}}{\pi^4 \tilde{h}_0^3} \frac{1}{((k_x/\tilde{l}_m)^2 + (k_y/\tilde{w}_m)^2)^2 (\pi^2 \tilde{B}[(k_x/\tilde{l}_m)^2 + (k_y/\tilde{w}_m)^2] + \tilde{T})}.$$
(4.5)

Using the physical values noted in its caption, figure 4(a) presents the resulting steady-state deformation (4.1) along the \hat{x} axis for various values of k_x , with $k_y = 1$ and $\tilde{h}_m = 10 \,\mu\text{m}$, and clearly shows the reduction in deformation magnitude as the wavenumber increases. Furthermore, (4.3) and (4.5) indicate that the scaling of the amplitude \tilde{d}_0 and time scale $\tilde{\tau}_0$ with the wavenumber depends on the relative contribution of the bending and tension terms in the denominator.

When $\pi^2 \tilde{B} k_x^2 \ll \tilde{T} \tilde{l}_m^2$, pre-stretching is dominant over bending forces and the deformation \tilde{d}_0 and time scale $\tilde{\tau}_0$ scale as k_x^{-3} and k_x^{-4} , respectively. However, when $\pi^2 \tilde{B} k_x^2 \gg \tilde{T} \tilde{l}_m^2$, bending is dominant, and the deformation and time scale decrease as k_x^{-5} and k_x^{-6} , respectively. From the definition of \tilde{B} , the condition for pre-stretching dominance can be expressed as $\pi^2 \tilde{E}_Y \tilde{h}_m^3 k_x^2 / 12(1 - \nu^2) \tilde{T} \tilde{l}_m^2 \ll 1$. Figure 4(*b,c*) presents the maximum deformation and the time scale as a function of k_x , respectively, for three values of the membrane thickness, \tilde{h}_m , showing that the deformation of a 10 μ m thick sheet scales as k_x^{-3} throughout the investigated range, whereas the time scale scales as k_x^{-4} . As the membrane thickness increases, the bending effect becomes apparent and for $\tilde{h}_m = 100 \ \mu$ m the amplitude and the time scale decrease as k_x^{-3} and k_x^{-4} for sufficiently low k_x values, but settle on a k_x^{-5} and k_x^{-6} dependence for high wavenumbers. For $\tilde{h}_m = 1$ mm, the bending effect is dominant and thus the amplitude and the time scale decrease as k_x^{-3} and the time scale decrease as k_x^{-5} and k_x^{-6} dependence for high wavenumbers. We note that for the set of parameters chosen here, even the first modes corresponding to the largest deformation satisfy the small-deformation requirement of the model.

5. Effect of discretized actuation on the deformation field

Equation (2.13) may be solved to obtain the actuation field required to achieve pre-defined deformation patterns of elastic plates, which may be desired in engineering applications. However, implementation of the resulting continuous actuation distribution may be challenging in practice. We here consider a discrete actuation profile, consisting of $D \times D$ individual squares, and seek to minimize the error between the resulting and desired deformation, for a given level of discretization. Specifically, actuating square *i* with amplitude a_i yields a deflection $a_i d_i(x, y)$ given by (3.2*a*), such that the resulting deformation is $\sum_{i=1}^{D^2} a_i d_i(x, y)$. For a given desired deformation d(x, y), we follow a least-squares method (Bjorck 1996) and seek to minimize the error

$$\int_{0}^{l_{m}} \int_{0}^{w_{m}} \left(\sum_{i,j=1}^{D^{2}} a_{i}d_{i} - d \right)^{2} \mathrm{d}x \, \mathrm{d}y = \sum_{i,j=1}^{D^{2}} a_{i}a_{j}\mathbf{A}_{i,j} - 2\sum_{i=1}^{D^{2}} a_{i}b_{i} + c,$$
(5.1)

where

$$\mathbf{A}_{i,j} = \int_0^{l_m} \int_0^{w_m} d_i d_j \, \mathrm{d}x \, \mathrm{d}y, \quad b_i = \int_0^{l_m} \int_0^{w_m} d_i d \, \mathrm{d}x \, \mathrm{d}y, \quad c = \int_0^{l_m} \int_0^{w_m} d^2 \, \mathrm{d}x \, \mathrm{d}y. \quad (5.2a-c)$$

Differentiating (5.1) with respect to each a_i and equating to zero yields the optimality condition

$$\mathbf{A}\mathbf{a} = \mathbf{b},\tag{5.3}$$

where $\boldsymbol{a} = [a_1, a_2, \ldots, a_{D^2}]^T$, $\boldsymbol{b} = [b_1, b_2, \ldots, b_{D^2}]^T$ and \boldsymbol{A} is a symmetric $D^2 \times D^2$ matrix with rank $D^2 - D$ and thus is not invertible (singular). The singularity of \boldsymbol{A} stems from the fact that the source term in (2.13) depends on gradients of the actuation field, thus allowing an associated gauge freedom in the choice of actuation (coefficients a_i) without modifying the resulting deformation. Specifically, for the case of a driving force f_{F_x} acting in $\hat{\boldsymbol{x}}$ the direction, it follows that adding an arbitrary

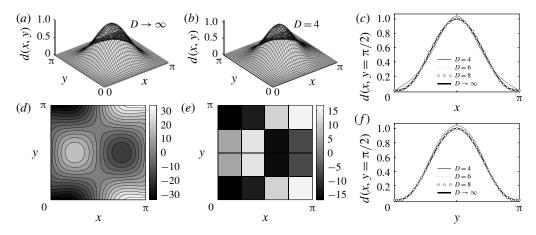


FIGURE 5. The effect of actuation discretization on the shape and the magnitude of the deformation. (a) Deformation formed by the continuous driving force f_{F_x} shown in (c), acting in the \hat{x} direction. (b) Deformation obtained from 4×4 square-shaped actuation regions, each having a uniform value which is found by solving the least-squares problem (5.3) and shown in (d). (e,f) Deformation along the \hat{x} and \hat{y} axes, respectively, for different levels of discretization.

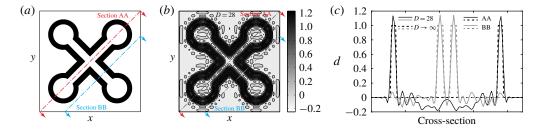


FIGURE 6. (Colour online) Demonstration of the use of a least-squares discretization method for creation of a complex deformation. (a) Top view of a microfluidic configuration, in which black lines represent the confining walls, characterized by step-like behaviour. (b) The deformation field (colour map) obtained from 28×28 square-shaped actuation regions, each having a uniform value found by solving the least-squares problem (5.3). (c) Deformation along the two cross-sections, depicted in (a) and (b), showing that discretization results in undesired oscillations of the deformation field. Dashed and solid lines correspond to the chosen and obtained deformation, respectively.

function $f_0(y)$ to the driving force, which has D values in discrete form, will not modify the resulting deformation.

To determine the coefficients a_i , we first reduced the matrix **A** and vector **b** only to rows with corresponding non-zero eigenvalues of **A**, obtaining a $(D^2 - D) \times (D^2)$ matrix and a $(D^2 - D) \times (1)$ vector, respectively. We then solved the reduced system (5.3) and found the vector **a** using MATLAB's routine lsqminnorm (release R2017b, Mathworks, USA), which computes the minimum least-squares solution of the system. As an illustrative example, we consider a localized deformation,

$$d(x, y) = (2/\pi)^{12} x^3 (\pi - x)^3 y^3 (\pi - y)^3,$$
(5.4)

shown in figure 5(*a*), and for simplicity assume a membrane regime (dominant prestretching, $\lambda = 0$). Using (2.13), the continuous driving force f_{F_x} required to create this deformation (at steady state) is given by

$$f_{F_x}(x, y) = -\int_{\pi/2}^x \nabla_{\parallel}^4 d(x', y) \,\mathrm{d}x', \tag{5.5}$$

and shown in figure 5(c). Figure 5(d) shows the discretization of this field into 4×4 square-shaped regions, each assigned with a uniform value obtained from the least-squares method solution of (5.3). Figure 5(b) presents the resulting deformation obtained by superposition of solutions for individual squares (3.2), using the values for forcing shown in figure 5(d). Figure 5(e,f) presents the deformation along the \hat{x} and \hat{y} axes, respectively, for different levels of discretization. While, as expected, discretization results in undesired oscillations of the deformation field due to high wavenumbers which are unbalanced, even a relatively coarse discretization with D=4 allows maintaining of a fairly localized deformation, with amplitude only larger by 4% than the desired one. For higher levels of discretization (D=6 and D=8), the difference between the resulting and desired deformations is almost indistinguishable.

To challenge our method of solution, we consider the microfluidic configuration shown in figure 6(a), in which the deformation magnitude is dictated strictly by 0 and 1, represented in the figure by white and black colours, respectively. Clearly, the exact description of this deformation field requires an infinite number of wavenumbers which cannot be represented by a finite grid discretization. Nevertheless, the deformation obtained using 28×28 square-shaped actuation regions is able to reproduce the main features of the geometry as shown in figure 6(b), although with undesired oscillations. For further clarification, figure 6(c) presents the deformation along the two cross-sections, illustrated in figure 6(a,b), showing that the maximal and minimal deformations are approximately by 11% and 18% larger than the desired one, respectively.

6. Investigation of nonlinear effects

In the previous sections we restricted our analysis to a strongly pre-stretched elastic sheet, $\alpha \ll 1$, and small elastic deformations, $\beta \ll 1$, and solved the linear governing equation (2.13) for the deformation field. In this section, we relax these restrictions and explore the nonlinear effects arising from the hydrodynamic nonlinearity in the Reynolds equation, h^3 , and the nonlinear coupling between the tension and deformation in the Föppl-von Kármán equations. However, we limit our nonlinear analysis to positive deformations, d > 0. We first study theoretically the weakly nonlinear effect of internal tension on the deformation (§ 6.2) and then investigate numerically the nonlinear effects considering finite α and β (§ 6.3). To this end, we consider an axisymmetric geometry which allows reduction to a single spatial variable and thus greatly simplifies theoretical and numerical investigation. This simple case is useful in providing physical insight on the nonlinear effects of α and β on the deformation and tension field. We also note the analysis of the axisymmetric configurations is relevant to adaptive optics applications, in which the liquid within a circular microchamber, covered with a thin elastic membrane, is pressurized to deform the membrane forming a plano-convex microlens (Chronis et al. 2003).

6.1. Coupled Reynolds and nonlinear Föppl-von Kärmán equations

We consider a circular elastic sheet of radius \tilde{R}_m subjected to axisymmetric driving forces acting either through the pressure applied directly to the elastic sheet or through the non-uniform slip velocity in the fluid. For simplicity, we neglect the effect of bending and consider a membrane (tension-dominant) regime, $\lambda \ll 1$. Based on these assumptions, the deformations of the elastic membrane are described by the axisymmetric Föppl–von Kármán equations for the membrane (see Landau & Lifshitz 1959; Lister *et al.* 2013; Zheng, Griffiths & Stone 2015)

$$\tilde{p} = -\tilde{\nabla}_r \cdot (\tilde{T}_r \tilde{\nabla}_r \tilde{d}) + \tilde{p}_e, \tag{6.1}$$

and

$$\frac{1}{\tilde{r}}\frac{\partial}{\partial\tilde{r}}\left(\tilde{r}^{3}\frac{\partial\tilde{T}_{r}}{\partial\tilde{r}}\right) = -\frac{\tilde{E}_{Y}\tilde{h}_{m}}{2}\left(\frac{\partial\tilde{d}}{\partial\tilde{r}}\right)^{2},$$
(6.2)

where $\tilde{\nabla}_r = (\partial/\partial \tilde{r})\hat{r}$ is the gradient in polar coordinates, $\tilde{r} = \sqrt{\tilde{x}^2 + \tilde{y}^2}$ is the radial coordinate and $\tilde{T}_r(\tilde{r}, \tilde{t})$ is the radial tension resulting from both external and internal tension formed in the membrane.

We define the normalized radial coordinate $r = \tilde{r}/\tilde{l}$, radial tension $T_r = \tilde{T}_r/\tilde{T}$ and dimensionless size of the membrane $R_m = \tilde{R}_m/\tilde{l}$. Substituting the normalized variables into (6.1)–(6.2) and using the results of scaling analysis in § 2.1 we obtain the non-dimensional Föppl–von Kármán equations

$$p = -\nabla_r \cdot (T_r \nabla_r d) + p_e, \tag{6.3}$$

$$\frac{1}{r}\frac{\partial}{\partial r}\left(r^{3}\frac{\partial T_{r}}{\partial r}\right) = -\frac{1}{2}\alpha\left(\frac{\partial d}{\partial r}\right)^{2}.$$
(6.4)

Substituting (6.3) into the nonlinear Reynolds equation (2.11), we obtain

$$\frac{\partial d}{\partial t} + \nabla_r \cdot [h^3 \nabla_r [\nabla_r \cdot (T_r \nabla_r d)]] = -\nabla_r \cdot [hf_F] + \nabla_r \cdot [h^3 \nabla_r f_E].$$
(6.5)

The evolution equation (6.5) and the second Föppl–von Kármán equation (6.4) are twoway coupled nonlinear equations, governing the fluid–structure interaction, that should be solved at once to obtain both deformation and tension fields.

The governing equations (6.4) and (6.5) are supplemented by six boundary conditions. At the centre of the membrane, we require regularity of d(r, t) and $T_r(r, t)$

$$\frac{\partial d}{\partial r} = 0$$
 and $\frac{\partial T_r}{\partial r} = 0$ at $r = 0$. (6.6*a*,*b*)

We also assume a zero flux q at the origin, given by $q = r(-h^3\partial p/\partial r + (1/2)hu_{slip})$, that under assumptions of finite u_{slip} and $\partial p_e/\partial r$ at r = 0 from (6.1) implies

$$\lim_{r \to 0} rh^3 \frac{\partial}{\partial r} \left[\frac{1}{r} \frac{\partial}{\partial r} \left(rT_r \frac{\partial d}{\partial r} \right) \right] = 0.$$
(6.7)

At the edge of the membrane, we consider the following boundary conditions:

$$d = r\frac{\partial T_r}{\partial r} + (1 - \nu)(T_r - 1) = \frac{\partial}{\partial r}\left(rT_r\frac{\partial d}{\partial r}\right) = 0 \quad \text{at } r = R_m. \tag{6.8a-c}$$

The first two conditions (6.8*a*,*b*) correspond to no transverse displacement, and fixed horizontal displacement at an outer circular frame holding the membrane, respectively. The last condition (6.8*c*) is obtained, as previously, from the elastic balance (6.3) by assuming the fluidic and external pressures are both zero at the boundaries, $p = p_e = 0$.

6.2. Asymptotic analysis for weakly nonlinear effects due to induced tension

In this section, we use asymptotic analysis to study the weakly nonlinear effects arising from internal tension formed in the elastic sheet during the deflection. We apply asymptotic expansions to decouple the two-way coupled nonlinear equations (6.5) and (6.4), assuming small deformation and strong pre-stretching of the elastic membrane, and obtain a correction for the effect of induced internal tension.

Assuming small elastic deformations, $\beta = \tilde{d}^* / \tilde{h}_0 \ll 1$, we eliminate the hydrodynamic nonlinearity in the Reynolds equation and obtain

$$\frac{\partial d}{\partial t} + \nabla_r^2 [\nabla_r \cdot (T_r \nabla_r d)] = -\nabla_r \cdot f_F + \nabla_r^2 f_E.$$
(6.9)

For the case of strongly pre-stretched elastic membrane, $\alpha = \tilde{T}_{in}/\tilde{T} \ll 1$, we expand the deformation and the tension in powers of α

$$d = d^{(0)} + \alpha d^{(1)} + O(\alpha^2), \quad T_r = 1 + \alpha T_r^{(1)} + O(\alpha^2), \quad (6.10a,b)$$

where α is a small parameter satisfying max(ϵRe , Wo, ϵ^2 , β , λ) $\ll \alpha \ll 1$. Substituting (6.10) into the coupled governing equations (6.4) and (6.9), results in three one-way coupled linear equations for the leading-order deformation and the first-order correction for the deformation and tension fields. In appendix D of the supplementary material, we present a detailed derivation of the governing equations and the appropriate boundary conditions at each order, and provide closed-form solutions for the leading-order deformation for the tension.

Similarly to §3, as an illustrative example we consider the non-uniform electroosmotic slip velocity as a driving force and specifically focus on a spatially nonuniform actuation of the form

$$\boldsymbol{f}_{F}(\boldsymbol{r},t) = V_{r} \mathbf{J}_{1} \left(\frac{\chi_{n} \boldsymbol{r}}{R_{m}}\right) \boldsymbol{H}(t) \hat{\boldsymbol{r}}, \qquad (6.11)$$

corresponding to a zeta-potential distribution of $\zeta(r) = r J_1(\chi_1 r/R_m)$, subjected to a suddenly applied electric field V_r/r in the \hat{r} direction, where $J_1(\chi_n r/R_m)$ is the Bessel function of the first kind and of the first order, and χ_n is the *n*th root of $J_0(\chi_n) = 0$. In our analysis, we hereafter focus on the first root, $\chi_1 = 2.4048$.

Using the governing equations and closed-form solutions derived in appendix D of the supplementary material, we can obtain analytical solutions for $d^{(0)}(r, t)$ and $T_r^{(1)}(r, t)$ resulting from (6.11). The leading-order deformation field is

$$d^{(0)}(r,t) = -\frac{V_r R_m^3}{\chi_n^3} \mathbf{J}_0\left(\frac{\chi_n r}{R_m}\right) \left[1 - \exp\left(-\frac{\chi_n^4}{R_m^4}t\right)\right],\tag{6.12}$$

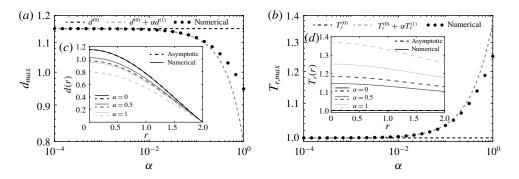


FIGURE 7. The effect of weak nonlinearity due to induced tension. (a,b) Comparison between asymptotic and numerical results for the maximum deformation and tension at steady state as a function of α . Dashed black and grey lines correspond to the leading- and first-order asymptotic solutions, respectively, while black dots correspond to the numerical solution. (c,d) Comparison between asymptotic (dashed lines) and numerical (solid lines) solutions for the steady-state deformation and tension, respectively, for $\alpha = 0$, 0.5 and 1. All calculations were performed using $\beta = 0$, $V_r = -2$, $\nu = 0.5$ and $R_m = 2$.

while the first-order correction for tension distribution reads

$$T_r^{(1)}(r,t) = \frac{V_r^2 R_m^4}{4\chi_n^4} \left[\frac{\nu J_1(\chi_n)^2}{1-\nu} + J_0(\bar{r})^2 + J_1(\bar{r})^2 - \frac{J_0(\bar{r}) J_1(\bar{r})}{\bar{r}} \right] \left[1 - e^{-(\chi_n^4/R_m^4)t} \right]^2, \quad (6.13)$$

where $\bar{r} = \chi_n r/R_m$. The maximum value $T_{r,max}^{(1)}$ is obtained at the centre of the membrane

$$T_{r,max}^{(1)} = \frac{V_r^2 R_m^4}{4\chi_n^4} \left[\frac{\nu J_1(\chi_n)^2}{1-\nu} + \frac{1}{2} \right].$$
(6.14)

While it is difficult to obtain a closed-form solution for transient first-order deformation $d^{(1)}(r, t)$, the corresponding steady-state deformation depends solely on the spatial coordinate and admits a closed-form solution

$$d_s^{(1)}(r) = \int_r^{R_m} T_{r,s}^{(1)} \frac{\mathrm{d}d_s^{(0)}}{\mathrm{d}\xi} \,\mathrm{d}\xi, \qquad (6.15)$$

where the subscript *s* denotes the steady state.

Figure 7 summarizes the effect of weak nonlinearity due to induced tension on the deformation and tension resulting from the forcing (6.11). Figure 7(*a,b*) presents the maximum deformation and tension at steady state as a function of α . Dashed black and grey lines correspond to the leading- and first-order asymptotic solutions obtained from (6.12), (6.14) and (6.15), whereas black dots correspond to the numerical solution. While the leading-order deformation and tension are independent of α , the first-order correction and numerical solution clearly show the reduction in deformation magnitude and the increase in the resulting tension, respectively, as the parameter α increases. In figure 7(*c*,*d*) we compare the asymptotic (dashed lines) and numerical (solid lines) solutions for the steady-state deformation and tension fields in the case of $\alpha = 0, 0.5$ and 1, showing good agreement. As can be inferred from the results of figure 7, for $\alpha \ll 1$ the first-order asymptotic solutions (6.13) and (6.15) accurately

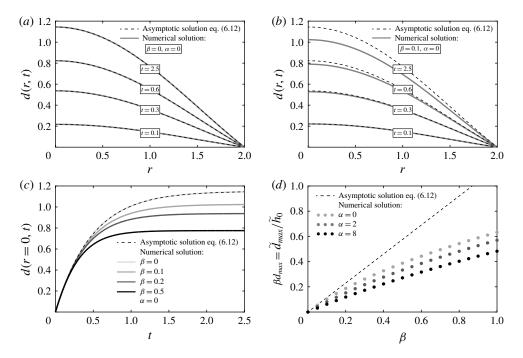


FIGURE 8. Investigation of nonlinear effects on the transient behaviour and the magnitude of deformation. (a,b) The time evolution of the deformation field for $\beta = 0$ (a) and $\beta = 0.1$ (b), in the case of a strongly pre-stretched elastic membrane, $\alpha = 0$. Grey solid lines represent the numerical results and black dashed lines represent the leading-order asymptotic solution (6.12). (c) The maximum deformation, obtained at the centre of the membrane, as a function of time for various values of β , with $\alpha = 0$. (d) The maximum deformation, in dimensional form, scaled by the initial fluid thickness, $\tilde{d}_{max}/\tilde{h}_0 = \beta d_{max}$ as a function of the parameter β , for various values of α . In (c,d) solid lines and dots represent the numerical results, respectively, and the dashed black curve represents the asymptotic solution (6.12). All calculations were performed using $V_r = -2$, $\nu = 0.5$ and $R_m = 2$.

describe the behaviour of the deformation and tension fields, but as α approaches and passes O(1) the asymptotic solutions overpredict them. Nevertheless, d_{max} and $T_{r,max}$ continue to decrease/increase monotonically with α and for $\alpha \gg 1$ scale like $\alpha^{-1/3}$ and $\alpha^{1/3}$, respectively, as shown by the nonlinear investigation in figure 9.

6.3. Numerical investigation of nonlinear effects

To investigate the nonlinear effects of finite α and β on the deformation and tension field, we proceed with a numerical analysis of the viscous-elastic governing equations (6.4)-(6.5). To study the effect of hydrodynamic nonlinearity (h^3) on the transient behaviour and on the magnitude of deformation, we consider for simplicity the case of a strongly pre-stretched elastic membrane with $T_r = 1$ ($\alpha = 0$) and solve numerically the nonlinear evolution equation (6.5) for the deformation using finite differences. In addition, to explore the combined effect of internal tension and hydrodynamic nonlinearity on the steady-state behaviour, we solve numerically the corresponding steady-state boundary value problem (6.4)-(6.5) subject to the six boundary conditions (6.6)-(6.8*a*-*c*) using MATLAB's routine bvp4c. Further details

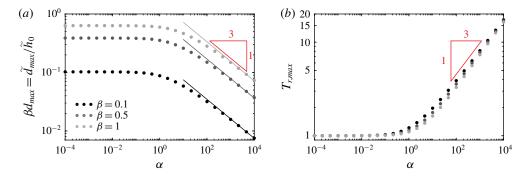


FIGURE 9. (Colour online) Investigation of nonlinear effect of the induced tension on the maximum displacement and tension. (a,b) Maximum displacement, $\beta d_{max} = h_{max} - 1 = \tilde{d}_{max}/\tilde{h}_0$ and tension, $T_{r,max}$, as a function of α , for $\beta = 0.1$, 0.5 and 1, obtained from numerical solution of (6.4)–(6.5). For $\alpha \ll 1$, both deformation and tension are independent of α , while for $\alpha \gg 1$ the deformation decreases as $\alpha^{-1/3}$ and the tension increases as $\alpha^{1/3}$. All calculations were performed using $V_r = -2$, $\nu = 0.5$ and $R_m = 2$.

of the numerical procedures and their cross-validation are discussed in appendix E of the supplementary material.

As shown in figure 8(*a*), we first validate our time-dependent numerical solver by comparing the numerically determined deformation field (solid lines) for $\alpha = \beta = 0$ with the leading-order asymptotic solution (6.12) (dashed lines), showing very good agreement for all times. Figure 8(*b*) presents the time evolution of the deformation profile (solid lines), for $\beta = 0.1$ and $\alpha = 0$. Figure 8(*c*) shows the time evolution of the maximum deformation, obtained at the centre of the membrane, for $\beta = 0, 0.1, 0.2, 0.5$ and $\alpha = 0$. Solid lines represent the numerical results, whereas dashed lines represent the leading-order asymptotic solution (6.12). It follows from figure 8(*b*,*c*) that as β increases the resulting maximum deformation in dimensionless form decreases. This behaviour can be explained as follows: since the viscous resistance scales as $h^{-3} = (1 + \beta d)^{-3}$, the increase in β leads to lower internal pressure gradient and thus lower deformation.

Figure 8(d) presents the scaled maximum deformation βd_{max} as a function of β , where the dots represent the numerical results for $\alpha = 0, 2, 8$, and the dashed curve represents the asymptotic solution (6.12), corresponding to $\alpha = \beta = 0$. We note that when exploring the nonlinear effects on the resulting magnitude of maximum deformation it is more convenient to discuss βd_{max} rather than d_{max} , since the former can be expressed as $\beta d_{max} = h_{max} - 1 = \tilde{d}_{max}/\tilde{h}_0$, representing the relative magnitude of \tilde{d} in terms of the initial fluid thickness, \tilde{h}_0 . The numerical analysis reveals that the scaled maximum deformation $\tilde{d}_{max}/\tilde{h}_0$ increases nonlinearly with β throughout the investigated range, showing a sub-linear behaviour, which is more pronounced as α increases. Physically, this means that when \tilde{d} becomes comparable to \tilde{h}_0 , the dependence of the deformation on the applied electric field is no longer linear due to internal tension and reduction in pressure, resulting in deformation that is lower than predicted by the linear response. However, in the small-deformation and strong pre-stretching limits, $\tilde{d}_{max}/\tilde{h}_0$ increases linearly with β , consistent with the leading-order asymptotic solution (6.12) (dashed line). Furthermore, figure 8(d) shows that, as expected, (6.12) reasonably predicts the maximum deformation, yielding modest relative error $(|(d_{max}^{num} - d_{max}^{(0)})/d_{max}^{num}| \lesssim 12\%)$ for up to $\beta = 0.1$.

Figure 9 illustrates the nonlinear effect of induced tension on the scaled maximum deformation and tension for different values of β . It is evident that at small values of α , corresponding to strong pre-stretching, the resulting maximum deformation and tension are almost independent of α , up to $\alpha = O(1)$ (see also figure 7). For $\alpha \gg 1$ and $\beta \lesssim 1$, performing scaling analysis of (6.4)–(6.5) (with $r \sim 1$), we obtain $T_r \sim \alpha d^2$ and $T_r d \sim V_r$ thus yielding

$$d \sim V_r^{1/3} \alpha^{-1/3}$$
 and $T_r \sim V_r^{2/3} \alpha^{1/3}$ for $\alpha \gg 1, \beta \lesssim 1$, (6.16*a*,*b*)

which is consistent with the numerical results shown in figure 9. As expected, for $\beta \leq 1$ the resulting maximum tension $T_{r,max}$ indicates weak dependence on β over the entire range of values of the parameter α , as shown in figure 9(*b*).

7. Concluding remarks

In this work, we examined the effect of pre-stretching and finite boundaries on the elastohydrodynamics of an elastic sheet lying on top of a thin liquid film. Assuming strong pre-stretching and small deformations of the lubricated elastic sheet, we used the linearized Reynolds and Föppl–von Kármán equations to derive general analytical solutions describing the deformation in a finite domain due to external forces. These closed-form solutions for realistic configurations allow one to study the relationship between the magnitude, time scale and resolution of elastic deformations, as well as to examine spatially discretized actuation. The asymptotic analysis of weakly nonlinear effect due to induced tension for the case of an axisymmetric configuration showed that the first-order asymptotic solutions for the deformation and tension field accurately capture the nonlinear trend even for α of O(1).

We obtained that in the small-deformation $(\tilde{d} \ll \tilde{h}_0)$ and strong pre-stretching $(\tilde{T}_{in} \ll \tilde{T})$ limits, the scaling $\tilde{d} \sim \tilde{\epsilon} \tilde{\zeta} \tilde{E} \tilde{l}^{*3} / \tilde{T} \tilde{h}_0^2$ (obtained from (2.6) combined with (2.8)) is appropriate, showing a linear relation between \tilde{d} and \tilde{E} , and may be used to estimate the resulting deformation. However, this linear dependence of the deformation on the applied forcing breaks down as \tilde{d} becomes comparable to \tilde{h}_0 , indicating a sub-linear behaviour, which is more pronounced as $\alpha = \tilde{T}_{in}/\tilde{T}$ increases.

While our main focus was on actuations applied by the fluid (specifically by non-uniform electro-osmotic flow), the governing equation (2.12) can be readily utilized to investigate the viscous–elastic dynamics due to forces applied directly on the elastic sheet. For such actuation, as shown by the Reynolds equation (2.11), the viscous flow arises only from temporal variation of the solid deformation field. Fluid velocity and gauge pressure vanish as the deformation reaches steady state. This is in contrast to the steady state of forcing applied to the fluid, which involves both non-zero fluid velocity and gauge pressure. Furthermore, with appropriate modification of the boundary conditions (e.g. prescribing an external pressure drop), the theoretical model we presented can be readily extended to the study of fluid–structure interaction in elastic microfluidic chips, where micro-channel flow may be driven, for example, by external pressure gradients or peristaltic actuation.

Actuation at the microscale is currently implemented mostly using microelectromechanical technologies, characterized by discrete and rigid elements. The presented results lay the theoretical foundation for implementation of actuation mechanisms based on low Reynolds number fluid-structure interaction. While our analysis focused on small deformations, we believe it may be directly useful for the design of soft and continuous actuators. For example, relevant deformations in configurable optics would be of the order of a wavelength (i.e. <1 μ m in the visible spectrum), and thus could be well described by our model when implemented on a 10 μ m liquid layer. Similarly, the field of microfluidics would highly benefit from configurable microstructures of the order of 10 μ m, which may be implemented on a 100 μ m thick liquid layer.

Acknowledgements

This project has received funding from the European Research Council (ERC) under the European Union's Horizon 2020 Research and Innovation Programme, grant agreement no. 678734 (MetamorphChip). We gratefully acknowledge support by the Israel Science Foundation (grant no. 818/13). E.B. is supported by the Adams Fellowship Program of the Israel Academy of Sciences and Humanities.

Author contributions

E.B. performed the theoretical and numerical research. E.B., A.D.G. and M.B. conceived the project, analysed the results and wrote the manuscript. R.E., E.B., K.G. and M.B. designed the experiments. R.E. and K.G. fabricated the experimental device. R.E. performed the experiments, analysed experimental data and wrote the experimental section.

Supplementary movies

Supplementary movies are available at https://doi.org/10.1017/jfm.2018.967.

REFERENCES

- AL-HOUSSEINY, T. T., CHRISTOV, I. C. & STONE, H. A. 2013 Two-phase fluid displacement and interfacial instabilities under elastic membranes. *Phys. Rev. Lett.* 111 (3), 034502.
- ARUTKIN, M., LEDESMA-ALONSO, R., SALEZ, T. & RAPHAËL, E. 2017 Elastohydrodynamic wake and wave resistance. J. Fluid Mech. 829, 538–550.
- BJORCK, A. 1996 Numerical Methods for Least Squares Problems. SIAM.
- CHRISTOV, I. C., COGNET, V., SHIDHORE, T. C. & STONE, H. A. 2018 Flow rate-pressure drop relation for deformable shallow microfluidic channels. J. Fluid Mech. 841, 267-286.
- CHRONIS, N., LIU, G. L., JEONG, K. H. & LEE, L. P. 2003 Tunable liquid-filled microlens array integrated with microfluidic network. *Opt. Express* **11** (19), 2370–2378.
- DENDUKURI, D., GU, S. S., PREGIBON, D. C., HATTON, T. A. & DOYLE, P. S. 2007 Stop-flow lithography in a microfluidic device. *Lab on a Chip* 7 (7), 818–828.
- GERVAIS, T., EL-ALI, J., GÜNTHER, A. & JENSEN, K. F. 2006 Flow-induced deformation of shallow microfluidic channels. *Lab on a Chip* 6 (4), 500–507.
- GROTBERG, J. B. & JENSEN, O. E. 2004 Biofluid mechanics in flexible tubes. Annu. Rev. Fluid Mech. 36, 121–147.
- GROVER, W. H., IVESTER, R. H. C., JENSEN, E. C. & MATHIES, R. A. 2006 Development and multiplexed control of latching pneumatic valves using microfluidic logical structures. *Lab on* a Chip 6 (5), 623–631.
- HARDY, B. S., UECHI, K., ZHEN, J. & KAVEHPOUR, H. P. 2009 The deformation of flexible PDMS microchannels under a pressure driven flow. *Lab on a Chip* **9** (7), 935–938.
- HEWITT, I. J., BALMFORTH, N. J. & DE BRUYN, J. R. 2015 Elastic-plated gravity currents. *Eur. J. Appl. Maths* **26** (01), 1–31.
- HOSOI, A. E. & MAHADEVAN, L. 2004 Peeling, healing, and bursting in a lubricated elastic sheet. *Phys. Rev. Lett.* **93** (13), 137802.

- HOWELL, P., KOZYREFF, G. & OCKENDON, J. 2009 Applied Solid Mechanics. Cambridge University Press.
- HUNTER, R. J. 2000 Foundations of Colloid Science. Oxford University Press.
- JEONG, K. H., LIU, G. L., CHRONIS, N. & LEE, L. P. 2004 Tunable microdoublet lens array. Opt. Express 12 (11), 2494–2500.
- KIM, S., LASCHI, C. & TRIMMER, B. 2013 Soft robotics: a bioinspired evolution in robotics. Trends Biotechnol. 31 (5), 287–294.
- KODIO, O., GRIFFITHS, I. M. & VELLA, D. 2017 Lubricated wrinkles: Imposed constraints affect the dynamics of wrinkle coarsening. *Phys. Rev. Fluids* **2** (1), 014202.
- LANDAU, L. D. & LIFSHITZ, E. M. 1959 Theory of Elasticity. Pergamon.
- LEAL, L. G. 2007 Advanced Transport Phenomena: Fluid Mechanics and Convective Transport Processes. Cambridge University Press.
- LISTER, J. R., PENG, G. G. & NEUFELD, J. A. 2013 Viscous control of peeling an elastic sheet by bending and pulling. *Phys. Rev. Lett.* **111** (15), 154501.
- MICHAUT, C. 2011 Dynamics of magmatic intrusions in the upper crust: theory and applications to laccoliths on Earth and the Moon. J. Geophys. Res. 116 (B5), B05205.
- MUKHERJEE, U., CHAKRABORTY, J. & CHAKRABORTY, S. 2013 Relaxation characteristics of a compliant microfluidic channel under electroosmotic flow. *Soft Matt.* **9** (5), 1562–1569.
- PANDA, P., YUET, K. P., DENDUKURI, D., HATTON, T. A. & DOYLE, P. S. 2009 Temporal response of an initially deflected PDMS channel. *New J. Phys.* **11** (11), 115001.
- PENG, G. G., PIHLER-PUZOVIĆ, D., JUEL, A., HEIL, M. & LISTER, J. R. 2015 Displacement flows under elastic membranes. Part 2. Analysis of interfacial effects. J. Fluid Mech. 784, 512–547.
- PIHLER-PUZOVIĆ, D., ILLIEN, P., HEIL, M. & JUEL, A. 2012 Suppression of complex fingerlike patterns at the interface between air and a viscous fluid by elastic membranes. *Phys. Rev. Lett.* **108** (7), 074502.
- PIHLER-PUZOVIĆ, D., JUEL, A. & HEIL, M. 2014 The interaction between viscous fingering and wrinkling in elastic-walled Hele-Shaw cells. *Phys. Fluids* **26** (2), 022102.
- PIHLER-PUZOVIĆ, D., PÉRILLAT, R., RUSSELL, M., JUEL, A. & HEIL, M. 2013 Modelling the suppression of viscous fingering in elastic-walled Hele-Shaw cells. J. Fluid Mech. 731, 162–183.
- PROSPERETTI, A. 2011 Advanced Mathematics for Applications. Cambridge University Press.
- RUBIN, S., TULCHINKY, A., GAT, A. D. & BERCOVICI, M. 2017 Elastic deformations driven by non-uniform lubrication flows. J. Fluid Mech. 812, 841-865.
- SHEPHERD, R. F., ILIEVSKI, F., CHOI, W., MORIN, S. A., STOKES, A. A., MAZZEO, A. D., CHEN, X., WANG, M. & WHITESIDES, G. M. 2011 Multigait soft robot. Proc. Natl Acad. Sci. 108 (51), 20400–20403.
- THORSEN, T., MAERKL, S. J. & QUAKE, S. R. 2002 Microfluidic large-scale integration. *Science* **298** (5593), 580–584.
- TIMOSHENKO, S. & WOINKOWSKY-KRIEGER, S. 1987 Theory of Plates and Shells. McGraw-Hill.
- TULCHINSKY, A. & GAT, A. D. 2016 Transient dynamics of an elastic Hele-Shaw cell due to external forces with application to impact mitigation. *J. Fluid Mech.* **800**, 517–530.
- UNGER, M. A., CHOU, H. P., THORSEN, T., SCHERER, A. & QUAKE, S. R. 2000 Monolithic microfabricated valves and pumps by multilayer soft lithography. *Science* 288 (5463), 113–116.
- ZHENG, Z., GRIFFITHS, I. M. & STONE, H. A. 2015 Propagation of a viscous thin film over an elastic membrane. J. Fluid Mech. 784, 443–464.