

Original Article

Magnetic resonance imaging-guided surgical design: can we optimise the Fontan operation?

Christopher M. Haggerty,¹ Ajit P. Yoganathan,¹ Mark A. Fogel^{2,3}

¹The Wallace H. Coulter Department of Biomedical Engineering, Georgia Institute of Technology & Emory University, Atlanta; ²Department of Pediatrics, Division of Cardiology; ³Department of Radiology, The Children's Hospital of Philadelphia, The University of Pennsylvania School of Medicine, Philadelphia, United States of America

Abstract The Fontan procedure, although an imperfect solution for children born with a single functional ventricle, is the only reconstruction at present short of transplantation. The haemodynamics associated with the total cavopulmonary connection, the modern approach to Fontan, are severely altered from the normal biventricular circulation and may contribute to the long-term complications that are frequently noted. Through recent technological advances, spear-headed by advances in medical imaging, it is now possible to virtually model these surgical procedures and evaluate the patient-specific haemodynamics as part of the pre-operative planning process. This is a novel paradigm with the potential to revolutionise the approach to Fontan surgery, help to optimise the haemodynamic results, and improve patient outcomes. This review provides a brief overview of these methods, presents preliminary results of their clinical usage, and offers insights into its potential future directions.

Keyword: Fontan procedure; magnetic resonance imaging; computational modeling

THE FONTAN PALLIATION FOR SINGLE-VENTRICLE congenital heart defects¹ is associated with decreased life expectancy² and numerous long-term complications that reduce quality of life.³ There is evidence to suggest that the surgical design and haemodynamics of the total cavopulmonary connection, the modern approach to the Fontan procedure in which the caval veins are connected to the pulmonary arteries, may play a role in the cause or exacerbation of some of these complications. For example, pulmonary arteriovenous malformations may develop from a lack of hepatic factors in the pulmonary blood supply,⁴ such as when there is preferential streaming of inferior venous flow through the Fontan baffle to a single lung.^{5,6} Thus, achieving a balanced distribution of blood flow

through the Fontan baffle to the pulmonary arteries is an important consideration in the surgical design. The haemodynamic power loss through the total cavopulmonary connection is also important given that elevated power loss – that is, inefficient flow through the connection – has been associated with decreased exercise capacity,⁷ ventricular preload, and cardiac output.⁸ These losses have also been shown to be sensitive to the surgical design of the Fontan connection, such as vessel size,⁹ connection angle,¹⁰ or choice of baffle design.^{11,12}

Despite the importance of optimising Fontan haemodynamics, the anatomic heterogeneity associated with single-ventricle heart defects precludes a “one-size-fits-all” approach to Fontan surgery. Instead, the connection design and patient-specific haemodynamics can vary considerably. Furthermore, the surgical design that is haemodynamically optimal may not be intuitively obvious, particularly in complex cases. Hence, there is a need for an advanced toolset that allows for visualisation of

Correspondence to: Dr Mark A. Fogel, MD, FACC, FAHA, FAAP, The Children's Hospital of Philadelphia, Division of Cardiology, 34th St. and Civic Center Blvd., Philadelphia, PA 19104, United States of America. Tel: +215 590 7566; Fax: +215 590 5825; E-mail: fogel@email.chop.edu

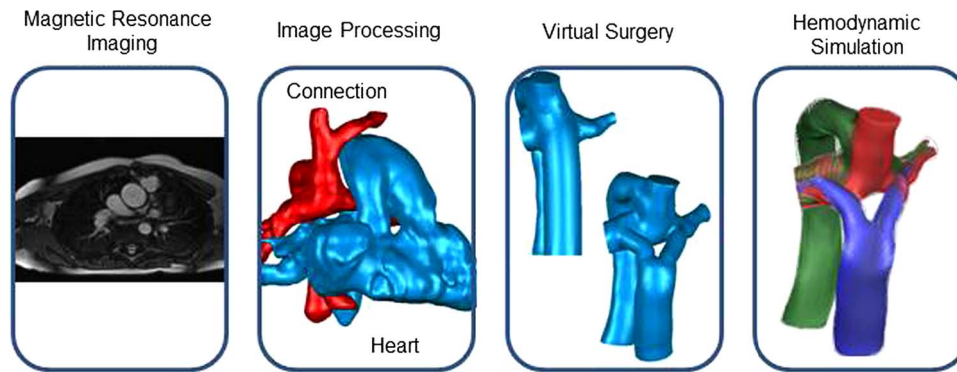


Figure 1.

Visual overview of the surgical planning workflow (from right to left): magnetic resonance imaging provides patient anatomy and flow information, which is extracted from post-processing. Virtual surgery enables the design of multiple connection options, which can then be evaluated with assistance from computational fluid dynamics simulations.

patient-specific connection options and can concurrently predict the haemodynamics associated with each option to facilitate selection of the optimal surgical approach. As a potential solution, a set of engineering tools in which cardiac magnetic resonance is used to inform computer-aided design and fluid dynamics simulations has been developed to assist in patient-specific surgical planning for the Fontan procedure. This review will provide a brief overview of these techniques, and highlight preliminary patient experiences.

Materials and methods

As shown in Figure 1, the surgical planning paradigm for Fontan surgery consists of four major steps: (1) medical image acquisition, (2) image processing to reconstruct the patient-specific anatomy, (3) virtual surgery, and (4) computational fluid dynamics simulations. The following sections will discuss each of these points in more detail, followed by a patient case study demonstrating their clinical usage.

Imaging and image processing: steps 1 and 2

Cardiac magnetic resonance is the modality of choice for this application given its ability to image the vascular anatomy and blood flow velocity, both without use of a contrast agent. For anatomic data, a contiguous stack of transverse “bright blood” images are acquired through the thorax (far left of Fig 1), and are used to reconstruct a three-dimensional model of the patient vessels – most often, the inferior and superior caval veins and the pulmonary arteries to their primary branches; second panel of Figure 1. This model serves as the input to both the virtual surgery software and the computational solver. The velocity data are acquired with phase contrast

imaging to measure the through-plane velocity. These data inform the computational flow solver as to the relevant blood flow rates into and out of the connection that are to be simulated, that is, they provide boundary conditions. Importantly, both the anatomic and velocity techniques described are already routine components of most cardiac magnetic resonance studies. Thus, the integration of image-guided surgical planning into clinical studies would not require additional scan time or trade-offs of other clinical data.

Finally, measurement of a four-dimensional flow field¹³ can also provide significant insights. Although not directly used in the surgical planning workflow, this *in vivo* flow information can be beneficial in cases with an existing “failed” Fontan connection to easily ascertain the adverse flow patterns that the new surgical connection must address. The study by Sundareswaran and de Zélicourt provides an excellent example of such a scenario.⁶

Virtual surgery and computational fluid dynamics simulations: steps 3 and 4

The virtual surgery tool provides a unique interface that takes in the reconstructed patient anatomy from medical imaging and uses free-form haptic devices to allow the user to position the surgical baffle in a three-dimensional space.¹⁴ The clinician can thus use this system to create and study the array of potential connection options under consideration for a given patient such as the comparison of an extracardiac conduit and a bifurcated Y-graft (third panel of Fig 1). Models of the surrounding anatomical structures, such as the heart, aorta, and pulmonary veins, are also included in the interface to provide relevant surgical landmarks. Comparison of the resulting Fontan models with post-operative

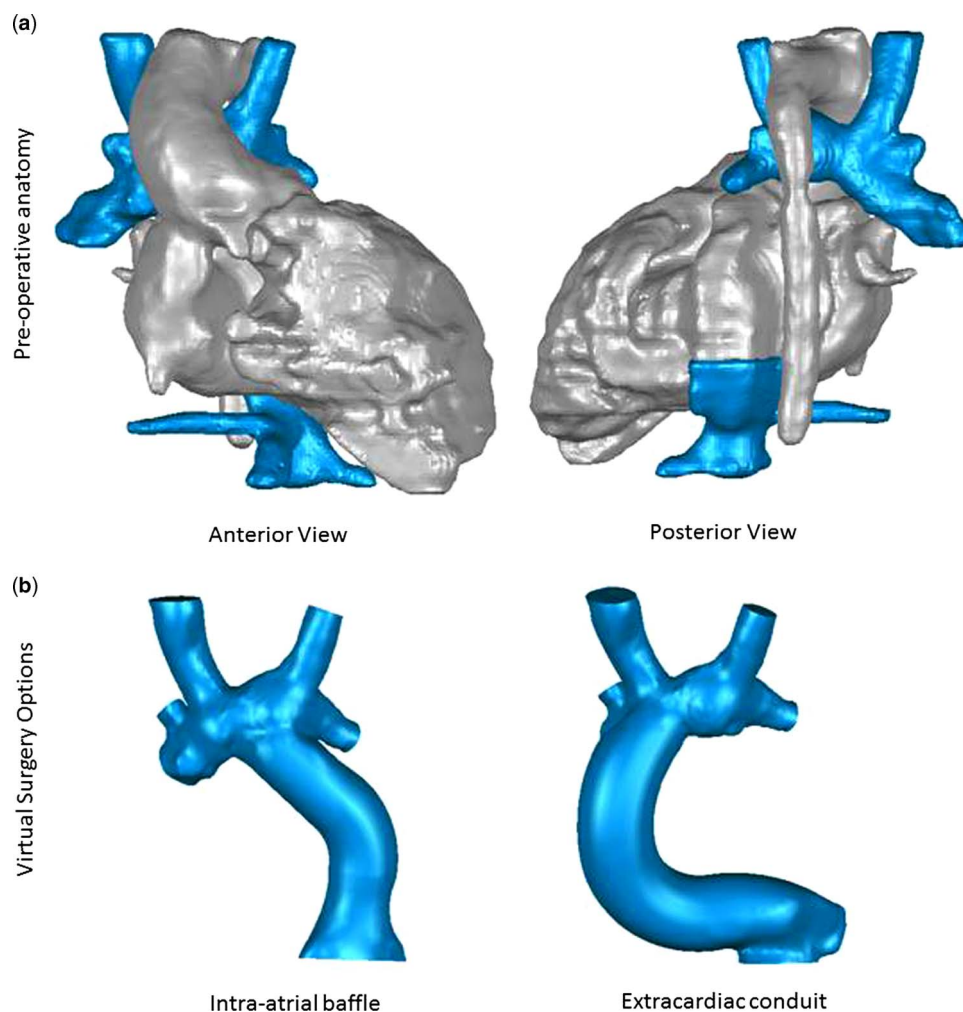


Figure 2.

(a) Anatomic reconstructions from patient case study. The heart and surrounding organs, which are included to provide surgical landmarks and points of reference, are coloured in grey, whereas the vessels that make up the Fontan connection are coloured blue. (b) Representative virtual surgery models considered for the patient: an intra-atrial baffle on the left, and an extracardiac connection on the right.

image reconstructions has shown that this tool can mimic these surgical connections with high fidelity.¹⁵

The final step is to simulate the local flow fields through each of the virtual connection models, quantify the relevant metrics of interest, and select the optimal surgical approach. Any validated fluid dynamics software package can be used for this analysis; our group primarily uses the custom solver developed by de Zélicourt et al¹⁶ Depending on the complexity of the connection, the size of the computational mesh, and the number of computational nodes used to run the solver, a single simulation can be completed on the order of hours to days. The result of the simulation is a high-resolution velocity field from which power loss, local flow distributions, or any other relevant metric of interest can be derived.

Case study

The following case example of a 2-year-old boy with heterotaxy syndrome of asplenia type who has undergone bilateral bidirectional Glenn illustrates the procedure and issues faced. Pulmonary arteriovenous malformations were suspected in the right lung. The primary challenge in the surgical approach to this patient, as shown in the anatomic reconstruction in Figure 2a, was the left-sided positioning of the inferior caval vein. Hence, the primary modelling objective was to identify the optimal approach to baffling the inferior caval flow to the pulmonary arteries that (a) ensured sufficient flow from the inferior caval vein to the right lung, and (b) minimised power losses.

Six different surgical options and three flow conditions were simulated; only the major findings are highlighted here. As shown in Figure 2b,

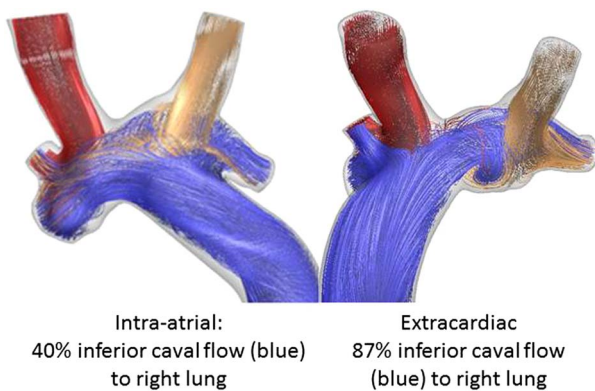


Figure 3.
Flow streaming results from computational fluid dynamics simulations for the considered surgical options. Flow from the inferior veins is coloured blue.

the surgical approach was ultimately a decision between a left-sided intra-atrial baffle (16 mm) and an extracardiac conduit (18 mm) that traversed the inferior aspect of the right atrium before turning superiorly towards the bidirectional Glenn connection.

Figure 3 shows representative velocity streamlines for the two surgical models, simulated under the pre-operatively measured flow conditions. The streamlines are coloured by the vessel of origin to facilitate visualisation of flow streaming; flow through the baffle is coloured blue. In both cases, inferior caval vein flow was seen to divide between the two lungs; however, the extracardiac model with the baffle positioned further to the right favoured inferior caval vein flow to the right lung – the side with the malformations – to a greater extent (87% versus 40%, respectively). Furthermore, with a larger conduit and more streamlined flow through the connection, the right-sided extracardiac connection also had the lowest connection resistance (0.13 versus 0.20 wood Units). Hence, the extracardiac connection was ultimately selected for surgical implementation.

To summarise, this patient presented with both a clinically important single-ventricle complication – pulmonary arteriovenous malformation – and a particularly complex anatomical configuration of the great vessels, which both make for a challenging approach to create the optimal Fontan procedure. In this setting, the image-guided surgical planning simulations produced valuable clinical insights by (1) providing a means to virtually explore the options available and (2) evaluating those options to identify the best approach.

Result verification

Clearly, these novel methods can only provide relevant clinical insights if the results generated

are accurate representations of the post-operative haemodynamics. Although capturing the requisite post-operative data to make these important comparisons can be a challenge, preliminary findings have been promising. We recently reported an in-depth analysis of four such patient cases with pre- and post-operative data, inclusive of anatomic, vessel flow rate, power loss, and flow distribution comparisons.¹⁵ The conclusions of that study were that model representations of the surgical connections and the flow distribution results, which are critical in cases of pulmonary arteriovenous malformations, were accurate within the uncertainty introduced by acute changes in flow split to the left and right lungs. Other groups have reported similar challenges in accurately accounting for post-operative pulmonary flow splits.¹⁷ Our model predictions of power losses, although close, require continued development given significant sensitivities to minimum vessel dimensions and systemic venous flow rates and distributions. Continued method development and data collection are ongoing to implement these findings and improve predictive accuracy.

Future directions

Towards the stated goal of optimising the Fontan connection using image-guided surgery planning, there is still much more work to be done, but the experience thus far has demonstrated that it is an attainable goal. To this end, the following is a brief overview of where the future of this technology is heading.

Lumped parameter modelling

Lower-order computational models of the entire cardiovascular system, in addition to the full fluid dynamics model, can provide a more complete analysis of patient physiology.¹⁷ Lumped parameter models provide a means to evaluate cardiac function, prescribe dynamic and responsive boundary conditions for the fluid simulation, or evaluate the pressures in other critical organs such as the liver. Hence, the continued development of such systems, and using them in tandem with more complex models, is an active area of research for many groups.

Planning for growth

The great challenge of Fontan physiology is not improving the acute surgical outcomes but achieving good long-term results and avoiding chronic failure. Thus, to truly optimise the connection, the ability to predict how it will grow with the patient and adapt to changing physiologic demands will be an important but daunting task. Building imaging

libraries of current patients, inclusive of serial follow-up, is likely the best way to begin to approach this objective in order to understand the modelling challenges that must be incorporated.

Expanding clinical indications for image-guided surgical planning

Patients with pulmonary arteriovenous malformations represent the majority of surgical planning experience to date as there is a solid understanding of the coupling between a measurable haemodynamic endpoint – equal hepatic flow to both lungs – and the cure for the disease – increased systemic oxygen saturation. As research identifies similar relationships for other complications, it is likely that this surgical planning paradigm can be applied to more such cases. With that said, preliminary experiences, such as the work described by Mirabella et al,¹⁸ have begun to show what else is possible, such as investigating the effect of reopening a fenestration in a patient with elevated central venous pressure and gastrointestinal complications.

Test bed of innovation

Until such time as patients born with a single ventricle can be expected to have a normal quality and longevity of life, surgical innovation and refinement will continue. Image-guided surgery planning can play a very important role in that process by providing an early outlet to establish proof of concept for these new ideas. Recent experiences with the Fontan Y-Graft^{12,19} and flow bifurcation²⁰ serve as excellent examples of this capability. The clinical use of the Y-Graft in particular grew from several surgical planning cases in which such a design was predicted to produce a favourable outcome; it is now being evaluated for potential haemodynamic improvements on a broader set of patients.

Conclusions

Image-guided virtual surgery for the Fontan procedure is a new and exciting paradigm that has the potential to revolutionise cardiovascular surgery for patients born with a single ventricle. By leveraging routine clinical imaging data, this technique enables the clinician to virtually visualise and evaluate patient-specific treatment options before even entering the operating room. By combining these models with state-of-the-art computational tools, the haemodynamic implications of each surgical design can be evaluated. Given the complexity and importance of haemodynamics in the long-term health and viability of the single-ventricle circulation, these data represent important clinical insights. Much work is

needed to continue to develop and perfect these techniques, but one day they may help achieve the elusive goal of patient-specific haemodynamic optimisation.

Acknowledgements

The authors acknowledge Jarek Rossignac for development of the virtual surgery interface, Diane de Zélicourt for development and implementation of the computational fluid dynamics solver, and Thomas Spray, J. William Gaynor, Kirk Kanter, and Pedro del Nido for lending their expertise and surgical insights.

Financial Support

This work was supported by the National Heart, Lung, and Blood Institute of the National Institutes of Health (R01HL67622 and R01HL098252), and the American Heart Association (10PRE3720002).

Conflicts of Interest

Dr Fogel has a grant from Edwards Life Sciences, Siemens Medical Solutions, and is medical monitor for an imaging agent from Kereos. Drs Haggerty and Yoganathan have no disclosures.

References

- Fontan F, Baudet E. Surgical repair of tricuspid atresia. *Thorax* 1971; 26: 240–248.
- Khairy P, Fernandes SM, John E, et al. Long-term survival, modes of death, and predictors of mortality in patients with fontan surgery. *Circulation* 2008; 117: 85–92.
- Anderson PAW, Sleeper LA, Mahony L, et al. Contemporary outcomes after the Fontan procedure. *J Am CollCardiol* 2008; 52: 85–98.
- Duncan BW, Desai S. Pulmonary arteriovenous malformations after cavopulmonary anastomosis. *Ann Thorac Surg* 2003; 76: 1759–1766.
- De Zélicourt D, Haggerty CM, Sundareswaran KS, et al. Individualized computer-based surgical planning to address pulmonary arteriovenous malformations in patients with a single ventricle with an interrupted inferior vena cava and azygous continuation. *J Thorac Cardiovasc Surg* 2011; 141: 1170–1177.
- Sundareswaran K, de Zélicourt D, Sharma S, et al. Correction of pulmonary arteriovenous malformation using image based surgical planning. *JACC Imaging* 2009; 2: 1024–1030.
- Whitehead KK, Pekkan K, Kitajima HD, et al. Nonlinear power loss during exercise in single-ventricle patients after the fontan: insights from computational fluid dynamics. *Circulation* 2007; 116: I-165–I-171.
- Sundareswaran KS, Pekkan K, Dasi LP, et al. The total cavopulmonary connection resistance: a significant impact on single ventricle hemodynamics at rest and exercise. *Am J Physiol* 2008; 295: H2427–H2435.
- Dasi LP, Krishnankutty R, Kitajima H, et al. Fontan hemodynamics: importance of pulmonary artery diameter. *J Thorac Cardiovasc Surg* 2009; 137: 560–564.
- Enslay A, Lynch P, Chatzimavroudis GP, et al. Toward designing the optimal total cavopulmonary connection: an in vitro study. *Ann Thorac Surg* 1999; 68: 1384–1390.

11. Marsden AL, Bernstein AJ, Reddy VM, et al. Evaluation of a novel y-shaped extracardiac fontan baffle using computational fluid dynamics. *J Thorac Cardiovasc Surg* 2009; 137: 394–403.
12. Haggerty CM, Kanter KR, Restrepo M, et al. Simulating hemodynamics of the fontan y-graft based on patient-specific in vivo connections. *J Thorac Cardiovasc Surg* 2013; 145: 663–670.
13. Sundareswaran KS, Haggerty CM, de Zélicourt D, et al. Visualization of flow structures in fontan patients using 3-dimensional phase contrast magnetic resonance imaging. *J Thorac Cardiovasc Surg* 2011.
14. Pekkan K, Whited B, Kanter K, et al. Patient-specific surgical planning and hemodynamic computational fluid dynamics optimization through free-form haptic anatomy editing tool (SURGEM). *Med Biol Eng Comput* 2008; 46: 1139–1152.
15. Haggerty CM, de Zelicourt D, Restrepo M, et al. Comparing pre- and post-operative fontan hemodynamic simulations: implications for the reliability of surgical planning. *Ann Biomed Eng* 2012; 40: 2639–2651.
16. de Zélicourt D, Ge L, Wang C, et al. Flow simulations in arbitrarily complex cardiovascular anatomies – an unstructured cartesian grid approach. *Computers & Fluids* 2009; 38: 1749–1762.
17. Pennati G, Corsini C, Cosentino D, et al. Boundary conditions of patient-specific fluid dynamics modelling of cavopulmonary connections: possible adaptation of pulmonary resistances results is a critical issue for virtual surgical planning. *Interface Focus* 2011; 1: 297–307.
18. Mirabella L, Haggerty CM, Passerini T, et al. Treatment planning for a TCPC test case: a numerical investigation under rigid and moving wall assumptions. *Int J Num Method Biomed Eng* 2013; 29: 197–216.
19. Kanter KR, Haggerty CM, Restrepo M, et al. Preliminary clinical experience with a bifurcated y-graft fontan procedure – a feasibility study. *J Thorac Cardiovasc Surg* 2012; 144: 383–389.
20. Desai K, Haggerty CM, Kanter KR, et al. Haemodynamic comparison of a novel flow-divider Optiflo geometry and a traditional total cavopulmonary connection. *Interact Cardiovasc Thorac Surg* 2013; 7: 1–7.