

# Functional Connectivity Variations in Mild Cognitive Impairment: Associations with Cognitive Function

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## Abstract

Participants with mild cognitive impairment (MCI) have a higher likelihood of developing Alzheimer's disease (AD) compared to those without MCI, and functional magnetic resonance neuroimaging (fMRI) used with MCI participants may prove to be an important tool in identifying early biomarkers for AD. We tested the hypothesis that functional connectivity differences exist between older adults with and without MCI using resting-state fMRI. Data were collected on over 200 participants of the Rush Memory and Aging Project, a community-based, clinical-pathological cohort study of aging. From the cohort, 40 participants were identified as having MCI, and were compared to 40 demographically matched participants without cognitive impairment. MCI participants showed lesser functional connectivity between the posterior cingulate cortex and right and left orbital frontal, right middle frontal, left putamen, right caudate, left superior temporal, and right posterior cingulate regions; and greater connectivity with right inferior frontal, left fusiform, left rectal, and left precentral regions. Furthermore, in an alternate sample of 113, connectivity values in regions of difference correlated with episodic memory and processing speed. Results suggest functional connectivity values in regions of difference are associated with cognitive function and may reflect the presence of AD pathology and increased risk of developing clinical AD. (*JINS*, 2012, 18, 39–48)

**Keywords:** Mild cognitive impairment (MCI), Resting-state fMRI, Functional connectivity, Posterior cingulate cortex, Memory, Basal ganglia, Striatum

## INTRODUCTION

Alzheimer's disease (AD) currently affects an estimated 4.5 million persons in the United States (Hebert, Scherr, Bienias, Bennett, & Evans, 2003) and is predicted to affect more than 13.5 million persons by the year 2050 (Alzheimer's Association, 2009). In view of the heavy medical, social, and economic burdens of the disease, prevention is the best long-term strategy for addressing this significant public health problem. The identification of individuals at higher risk of developing a clinical diagnosis of AD is necessary for any comprehensive prevention program, and a variety of approaches have been used to identify predictive biomarkers

(Sperling et al., 2011). In particular, functional neuroimaging biomarkers have significantly advanced our understanding of the progression to AD (Habeck et al., 2008), and advanced neuroimaging techniques will play an even greater role in the diagnosis of early AD according to recently revised criteria (McKhann et al., 2011). One approach which shows particular promise in the early detection of AD uses resting-state functional magnetic resonance imaging (fMRI) to assess functional connectivity in the brain by detecting gray matter regions that exhibit high temporal correlation of low frequency fluctuations. Because participants are asked to simply lie still during a conventional MR scan, resting-state fMRI can be used outside of specialized academic medical centers and thus has potential to become a widely used clinical diagnostic tool.

Resting-state fMRI has been increasingly used as a method for ascertaining functional connectivity of portions of the

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Default Mode Network (Buckner et al., 2005, 2009; Buckner and Vincent, 2007; Fleisher et al., 2009; Greicius, Srivastava, Reiss, & Menon, 2004; Hedden et al., 2009; Koch et al., 2010; Sperling et al., 2009; Wang et al., 2006), a network of brain regions including the posterior cingulate cortex, ventral anterior cingulate cortex, lateral parietal, temporal, and medial frontal regions that consistently show greater activity during periods of rest and less activity during periods of active cognitive engagement (Damoiseaux et al., 2006; Greicius, Krasnow, Reiss, & Menon, 2003; Greicius et al., 2008; Gusnard & Raichle, 2001; Harrison et al., 2008; Raiche et al., 2001). Beta amyloid deposition, which increases the risk of cognitive decline and dementia in aging (Sperling et al., 2011), appears to be greater in regions that comprise the Default Mode Network demonstrated by imaging using <sup>11</sup>C-labeled Pittsburgh Compound B (Hedden et al., 2009; Sperling et al., 2009), and greater amyloid deposition in the Default Mode Network has been linked to worse performance in associative memory fMRI tasks in elderly controls and mild AD participants (Buckner et al., 2005).

Using resting-state fMRI to investigate functional connectivity in the Default Mode Network, several groups have shown less functional connectivity between the posterior cingulate and medial temporal regions in MCI and AD (Allen et al., 2007; Rombouts, Barkhof, Goekoop, Stam, & Sheltens, 2005; Sorg et al., 2007; Wang et al., 2006; Zhang et al., 2009; Zhou et al., 2008). However, some studies have found greater connectivity between the posterior cingulate cortex and frontal regions in persons with MCI (Bai et al., 2009) and others less connectivity (Gili et al., 2011), in addition to less connectivity between the posterior cingulate cortex and medial temporal lobe. The observation of increased functional connectivity between the posterior cingulate cortex and frontal regions suggests that as certain regions become functionally disconnected, other regions may become more functionally connected, perhaps as a compensatory response in older age. This is similar to what has been observed in some event-related fMRI studies (e.g., Cabeza, 2002).

Previous resting-state neuroimaging biomarker endeavors have focused on highly selected individuals with relatively low experimental group numbers. This focus may have contributed to the discrepant findings of prior studies. Furthermore, the use of highly selected individuals may limit generalization of this approach to the community where biomarker studies will be most widely used as a diagnostic tool. In the present study, we investigated differences in functional connectivity in persons with MCI compared to persons with no cognitive impairment participating in the Rush Memory and Aging Project, a community-based, clinical-pathological cohort study of aging and dementia (Bennett et al., 2005). We hypothesized that persons with mild cognitive impairment would show reductions in functional connectivity to the posterior cingulate cortex when compared to persons with no cognitive impairment. Furthermore, we hypothesized that functional connectivity values in regions of difference would correlate with measures of cognition.

## METHODS

### Participants and Procedures

Participants were recruited from the Rush Memory and Aging Project, a community-based clinical-pathologic cohort study of aging and dementia (Bennett et al., 2005). Participants are free of clinically diagnosed dementia at baseline and are followed annually until death. They come from approximately 40 residential facilities across the greater Chicago metropolitan area, including subsidized senior housing facilities, retirement communities, retirement homes, local churches, and other community organizations. All participant procedures were approved by an Internal Review Board.

The Rush Memory and Aging Project has a rolling admission that started in 1997. Brain imaging was initiated in 2008. At the time of analyses, 1299 participants had enrolled and completed their baseline evaluation, 443 died, and 77 refused further participation before scan data collection began. Of the remaining 779, a total of 260 had MRI contraindications or were unable to sign informed consent leaving 519 eligible for scanning. Of these, 155 (29.9%) refused, 214 were scanned, and the remaining 150 were still being scheduled for scanning. From the 214 that were scanned, 14 were dropped due to excessive motion, 7 were dropped due to scanning data acquisition problems, leaving 193 participants. Of these, 40 were found to have MCI (as described below), and 40 demographically matched participants without cognitive impairment (also described as “no cognitive impairment” or “NCI”) were selected at random by a statistician for initial analyses to determine peak voxels of difference. The remaining 113 non-cognitively impaired participants were used as an “alternate sample” to test the association between observed regions of difference (coordinates defined by between-group differences) and measures of cognition. The alternate sample was used to avoid any issues of multicollinearity, circularity, or selection bias since the MCI and non-cognitive impaired groups were distinguished by performance on cognitive measures.

Diagnostic classification was performed by a clinician with expertise in the evaluation of older persons after review of clinical data. A battery of 21 cognitive performance tests was administered by trained technicians in an approximately hour-long session during baseline and annual follow-up sessions. Measures of cognitive function assessed a broad range of dissociable cognitive abilities that are consistent with functioning of different anatomic substrates commonly affected by aging and AD (Bennett et al., 2006; Wilson, Barnes, & Bennett, 2003). Episodic memory measures included Word List Memory, Word List Recall and Word List Recognition from the procedures established by the CERAD; immediate and delayed recall of Logical Memory Story A and the East Boston Story. Semantic memory measures included Verbal Fluency, Boston Naming, subsets of items from Complex Ideational Material, and the National Adult Reading Test. Working memory measures included the Digit Span subtests (forward and backward) of the

Wechsler Memory Scale-Revised and Digit Ordering. Measures of perceptual speed included the oral version of the Symbol Digit Modalities Test and Number Comparison. Measures of visuospatial ability included Judgment of Line Orientation and Standard Progressive Matrices. Raw scores on each test were converted to standard z-scores using the mean and standard deviation from the baseline evaluation. A person's standard scores across 19 tests were averaged to yield a single overall cognitive composite score (Fleischman, Wilson, Bienias, & Bennett, 2005). A composite score for five cognitive domains (episodic memory, semantic memory, working memory, perceptual speed, visuospatial ability) was created by averaging the z-scores of all measures within a domain, as previously described (Fleischman et al., 2005). A composite score has the advantage of increasing power by reducing random variability and floor and ceiling effects. An experienced neuropsychologist with expertise in aging and AD and blinded to participant age, sex, and race reviewed all results of cognitive measures and rendered a judgment as to cognitive impairment. Next, an experienced clinician with expertise in the diagnosis of AD reviewed all available participant information (cognitive data, medical history, neurological exam, brain scan) and rendered a judgment as to dementia in accordance with NINCDS/ADRDA criteria. Finally, any participant with cognitive impairment but no dementia was deemed to have MCI (Bennett et al., 2002; Boyle, Wilson, Aggarwal, Tang, & Bennett, 2005). This diagnostic characterization of MCI by the Rush Alzheimer's Disease Center closely resembles the condition of "Cognitive Impaired Not Demented" or otherwise known as CIND (Graham et al., 1997).

### Image Acquisition and Processing

MRI scans were conducted on a 1.5 Tesla clinical scanner (General Electric, Waukesha, WI), equipped with a standard quadrature head coil, located within the community of the sample. High data quality was ensured through daily quality assurance tests. High-resolution T1-weighted anatomical images were collected with a 3D magnetization-prepared rapid acquisition gradient-echo (MPRAGE) sequence with the following parameters: repetition time (TR) = 6.3 ms; echo time (TE) = 2.8 ms; preparation time = 1000 ms; flip angle = 8°; 160 sagittal slices; 1 mm slice thickness; field of view (FOV) = 24 cm × 24 cm; acquisition matrix 224 × 192, reconstructed to a 256 × 256 image matrix; scan time = 10 min and 56 s. Two copies of the T1-weighted data were acquired on each subject. Resting-state MRI data was acquired using a two-dimensional (2D) spiral in/out echo-planar imaging (EPI) sequence with the following parameters: TR = 2000 ms; TE = 33 ms; flip angle = 85°; 26 oblique axial slices; 5 mm slice thickness; acquisition/reconstruction matrix 64 × 64; FOV = 24 cm × 24 cm; 240 time-points/volumes; scan time = 8 min. Participants were not given instructions regarding the opening and closing of eyes.

The skull was removed from each structural MRI dataset using FreeSurfer's Hybrid Watershed Algorithm (Segonne et al., 2004). Structural scans were also manually edited when necessary to remove residual non-brain material. Brain segmentation into gray matter, white matter and CSF was also performed using FreeSurfer (<http://surfer.nmr.mgh.harvard.edu/>). Whole brain volume was also derived, and thus proportions of each compartment were calculated.

The first five image volumes of resting-state data were discarded at the scanner to avoid using data collected before reaching signal equilibrium. Images were reconstructed on Linux machines from the acquired k-space data (Glover & Thomason, 2004). Using the Statistical Parametric Mapping software (Friston et al., 1995; <http://www.fil.ion.ucl.ac.uk/spm/>) version 8 (SPM8), all volumes were corrected for motion, co-registered to the high-resolution T1-weighted data, and spatially normalized to the Montreal Neurological Institute (MNI) template. The normalized image volumes were spatially smoothed with a 4-mm full-width half-maximum (FWHM) Gaussian kernel. Next, a band-pass filter of 0.01 to 0.08 Hz was applied to the data in temporal frequency space to minimize low-frequency signal drift and high frequency variations due to cardiac and respiratory effects. To remove any residual effects of motion and other non-neuronal factors, 6 head motion parameters, as well as parameters for the white matter signal, global mean signal, and cerebrospinal fluid signal were used as nuisance variables (Buckner et al., 2009) in functional connectivity analysis using the Resting-State fMRI Data Analysis Toolkit (REST: <http://restfmri.net/forum/REST>).

Previous research suggests that the functional connectivity map generated when using the posterior cingulate as a seed region of interest may provide the best match with the hypothesized Default Mode Network (Greicius et al., 2003; Buckner et al., 2009). Therefore, a spherical seed ROI with a radius of 4 mm was prescribed in the posterior cingulate cortex, with MNI coordinates of  $x = 0$ ,  $y = -53$ ,  $z = 26$  in accordance with previous work (Hedden et al., 2009). A mean signal time course for the seed was calculated and used as a reference. Cross-correlation analysis was then conducted between the reference signal time course and the time series of each other voxel in the brain. The voxels showing significant functional connectivity to the posterior cingulate seed ROI were identified as those voxels whose cross-correlation differed significantly ( $\alpha = 0.001$ ) from 0, based on whole-brain Fisher's z-transformation of the correlations at the individual level. Seed-based functional connectivity analysis was conducted with the Data Processing Assistant for Resting-State fMRI (DPARSF; <http://restfmri.net/forum/DPARSF>) and SPM8.

### Statistical Analyses

Statistical analyses proceeded in several steps. We first examined between-group differences in demographic variables (age, education, sex, Mini-Mental State Examination [MMSE], race), cognitive performance data (episodic memory,

semantic memory, working memory, processing speed, perceptual organization, global cognition), brain volumetry (total gray matter volume and posterior cingulate cortex volume), and clinical diagnosis (MCI *versus* no cognitive impairment) using between-group analyses (age, education, MMSE, total gray matter volume, posterior cingulate volume), or Chi-square tests (sex, race). We then verified the functional connectivity of the posterior cingulate cortex to other regions associated with the Default Mode Network by determining within-group whole brain z-transformed functional clusters of significance, for both clinical diagnoses (MCI and no cognitive impairment), after controlling for the effects of total gray matter volume. To control for multiple comparisons, within-group whole brain functional imaging results were controlled by using a false-discovery rate (FDR) of  $p < .01$ . After verifying the functional connectivity of the posterior cingulate cortex to other regions associated with the Default Mode Network, we conducted voxel-wise, between-group comparisons of z-transformed functional connectivity values (MCI *versus* no cognitive impairment) while adjusting for the effects of total gray matter volume. The chance of spurious findings was controlled by using a voxel height threshold of  $p < .001$  and a cluster size threshold of five voxels. Finally, in each subject of an alternate sample, we extracted functional connectivity z-scores at the same coordinates of the maximum intensity voxels of clusters of difference from our

between-group comparisons and conducted exploratory partial correlations of these connectivity z-scores with measures of cognitive performance. A non-cognitively impaired alternate sample was used for the partial correlation analyses to avoid any issues of multicollinearity, circularity, or selection bias since MCI and non-cognitively impaired participants were grouped based on cognitive performance. Partial correlations were adjusted for age, education, and gender as these factors have been known to correlate with cognitive performance. Significance was determined at  $p < .05$ .

## RESULTS

### Demographic, Cognitive, and Brain Volumetry Differences Between MCI and Those Without Cognitive Impairment

Demographic, cognitive, and brain volumetry characteristics are shown in Table 1. Most participants were white. As expected, persons with MCI had lower MMSE scores, but did not significantly differ in terms of age, sex, or education. Furthermore, persons with MCI had lower scores on the global cognition measure and all five cognitive domain scores. Total gray matter volume and posterior cingulate cortex volume did not differ significantly between groups.

**Table 1.** Statistics for demographic, cognitive, and brain volumetry variables for the non-cognitive impaired participants (NCI,  $N = 40$ ) and mild cognitively impaired participants (MCI,  $N = 40$ )

	NCI $n = 40$	MCI $n = 40$	Whole sample $n = 80$	$t$ or $\chi^2$	$p$ value
Age (years)					
Mean ( $SD$ )	86.28 (4.39)	86.26 (4.49)	86.27 (4.41)	.025	.98
Range	74–94	75–94	74–94		
Education (years)					
Mean ( $SD$ )	15.98 (2.86)	15.00 (3.22)	15.49 (3.07)	1.43	.16
Range	12–23	8–25	8–25		
MMSE (total score)***					
Mean ( $SD$ )	28.68 (1.23)	27.10 (1.96)	27.59 (1.81)	4.31	<.001
Range	26–30	23–30	23–30		
Sex					
% Female	62.5 ( $n = 25$ )	82.5 ( $n = 33$ )	72.5 ( $n = 58$ )	3.07	.08
Race					
% White	100 ( $n = 40$ )	100 ( $n = 40$ )	100 ( $n = 80$ )	–	–
Global Cognition (z-score)***	0.49 (0.41)	–0.18 (0.50)		6.59	<.001
Episodic Memory (z-score)***	0.68 (0.52)	–0.23 (0.85)		5.74	<.001
Semantic Memory (z-score)***	0.56 (0.63)	–0.07 (0.75)		4.02	<.001
Working Memory (z-score)**	0.31 (0.73)	–0.16 (0.83)		2.69	.009
Processing Speed (z-score)**	0.25 (0.63)	–0.16 (0.73)		2.70	.008
Perceptual Organization (z-score)***	0.45 (0.53)	–0.33 (0.91)		4.64	<.001
Total Gray Matter ( $\text{mm}^3$ )	268.10 (26.85)	270.34 (21.03)		–0.42	.68
Posterior Cingulate Cortex ( $\text{mm}^3$ )	2.98 (0.60)	3.04 (0.57)		–0.49	.62

*Note.* Data are summarized as Mean (standard deviation =  $SD$ ) or as number (%). Age and education are presented in years; MMSE is total score; global cognition, episodic memory, semantic memory, working memory, processing speed, and perceptual organization are presented as z-scores; and total gray matter and posterior cingulate cortex volumes are presented as  $\text{mm}^3$ . Asterisks indicate significant differences between diagnostic groups. \*\* $p < .01$  \*\*\* $p < .001$ .



## Resting-State Functional Connectivity Differences Between MCI and Those Without Cognitive Impairment

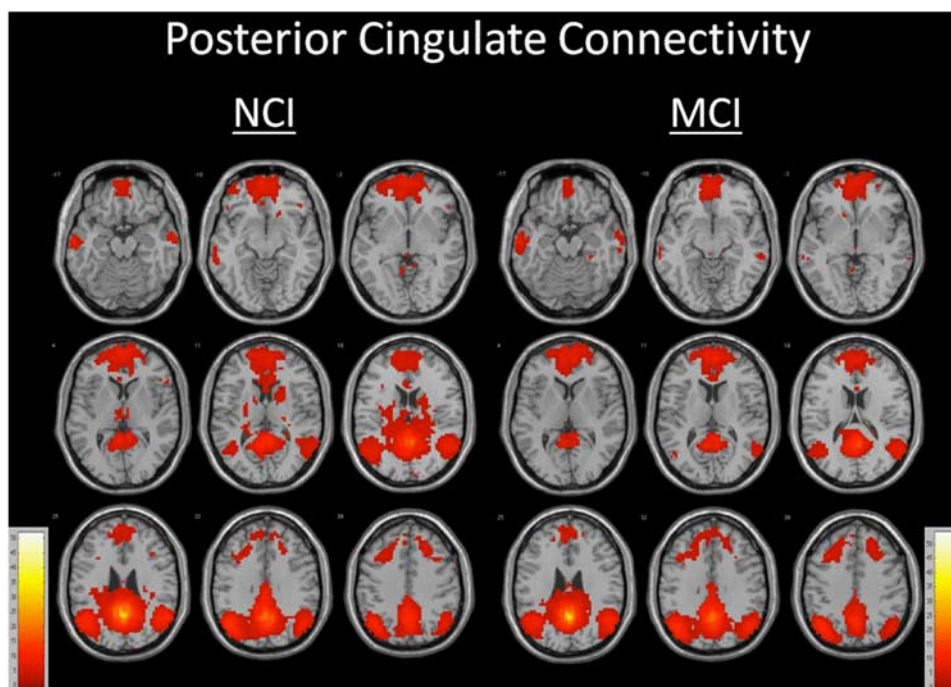
Seeding the posterior cingulate cortex yielded a network of functionally related regions consistent with the Default Mode Network in analyses controlling for total gray matter volume among cognitively intact and MCI participants in within-group analyses (Figure 1 and Table 2). These regions included large clusters of significance centering in widespread bilateral posterior cingulate, medial and lateral parietal, temporal, occipital, basal ganglia, and thalamic regions ( $t = 51.6306$ ), widespread bilateral medial frontal and anterior cingulate regions ( $t = 9.0885$ ), and smaller clusters of significance in left ( $t = 7.2618$ ;  $t = 4.2848$ ) and right ( $t = 6.7549$ ) middle temporal, left ( $t = 4.6772$ ) and right ( $t = 6.0595$ ;  $t = 4.5446$ ) cerebellum, left superior temporal ( $t = 4.9723$ ), left ( $t = 3.5388$ ) and right ( $t = 4.5782$ ) orbital frontal, right insula ( $t = 4.2836$ ), left ( $t = 4.2180$ ) and right ( $t = 3.9550$ ) thalamus, left brainstem ( $t = 4.1424$ ), right cuneus ( $t = 4.0907$ ), right caudate ( $t = 3.9912$ ), and left ( $t = 3.6707$ ) and right ( $t = 3.8836$ ;  $t = 3.7365$ ) inferior frontal regions for those without cognitive impairment. For participants with MCI, large clusters of significance were observed centering in widespread bilateral posterior cingulate, medial and lateral parietal, temporal, occipital, basal ganglia, and thalamic regions ( $t = 53.8787$ ), widespread bilateral medial, frontal, and anterior cingulate regions ( $t = 10.1883$ ), and smaller clusters of significance in the left ( $t = 7.9563$ ) and right ( $t = 7.4053$ ;  $t = 3.7045$ ;  $t = 3.9644$ ;  $t = 3.7045$ ) middle temporal, right

( $t = 6.5141$ ;  $t = 4.5733$ ;  $t = 4.3973$ ) and left ( $t = 6.4655$ ;  $t = 5.1676$ ;  $t = 4.2190$ ) cerebellum, right parahippocampal ( $t = 4.6878$ ), right superior temporal ( $t = 4.5437$ ), right thalamus ( $t = 4.3221$ ), left brainstem ( $t = 4.1668$ ), left caudate ( $t = 4.1087$ ), and right anterior cingulate ( $t = 3.8263$ ) regions.

Multiple regions of functional connectivity differences were observed between MCI and NCI subjects in between-group analyses (Figure 2 and Table 3). Persons with MCI were characterized by less functional connectivity in left ( $t = 4.2153$ ) and right ( $t = 3.9043$ ) orbital frontal, right middle frontal ( $t = 3.8609$ ), left putamen ( $t = 4.9792$ ), right caudate ( $t = 4.1524$ ;  $t = 4.0735$ ), left superior temporal ( $t = 3.9342$ ), and right posterior cingulate ( $t = 4.7002$ ) regions. By contrast, persons with MCI had greater functional connectivity in the left fusiform ( $t = 4.6011$ ), left rectal ( $t = 3.9158$ ), right inferior frontal ( $t = 3.8467$ ), and left precentral ( $t = 4.1251$ ) regions.

## Relationship Between Regions of Functional Connectivity Differences and Cognitive Performance

When exploring the relationship between cognition and connectivity values in the regions with functional connectivity differences, the level of connectivity correlated with measures of episodic memory and processing speed in three of the 12 regions in partial correlations that adjusted for age, education, and gender in an alternate group ( $N = 113$ ; Table 4) of non-cognitively impaired older adults (Table 5). Specifically, episodic memory domain z-scores correlated



**Fig. 1.** Functionally connected clusters indicated by a seed region of interest (ROI) prescribed in the posterior cingulate cortex for participants with no cognitive impairment (NCI,  $N = 40$ ) and participants with mild cognitive impairment (MCI,  $N = 40$ ). Seed ROI MNI coordinates:  $x = 0$ ,  $y = -53$ ,  $z = 26$ ; radius = 4 mm,  $p < .001$ , cluster size  $> 5$  voxels, false-discovery rate (FDR) corrected at  $p < .01$ .

**Table 2.** Functionally connected clusters as indicated by a seed region of interest (ROI) prescribed in the posterior cingulate cortex and covarying for the effects of total gray matter volume for non-cognitively impaired participants (NCI) and mild cognitive impaired participants (MCI)

Group	Region	Cluster Size (# voxels)	Maximum Intensity Voxel coordinates			t-value
NCI	Widespread bilateral posterior cingulate, medial and lateral parietal, temporal, occipital, basal ganglia, thalamus	5393	0	-54	27	51.6306
	Widespread bilateral medial frontal, anterior cingulate	2573	-3	63	0	9.0885
	L middle temporal	160	-63	-15	-18	7.2618
	R middle temporal	95	63	-9	-21	6.7549
	R cerebellum	90	6	-54	-42	6.0595
	L superior temporal	5	-39	21	-30	4.9723
	L cerebellum	74	-30	-78	-39	4.6772
	R orbital frontal	6	45	30	-12	4.5782
	R cerebellum	61	33	-75	-39	4.5446
	L middle temporal	5	-48	6	-36	4.2848
	R insula	5	36	-12	21	4.2836
	L thalamus	26	-9	-21	6	4.2180
	L brainstem	8	0	-33	-6	4.1424
	R cuneus	9	9	-93	21	4.0907
	R caudate	8	18	21	-6	3.9912
	R thalamus	12	6	-18	3	3.9550
	R inferior frontal	11	57	24	3	3.8836
	R inferior frontal	5	36	24	24	3.7365
	L inferior frontal	10	-51	24	6	3.6707
	L orbital frontal	6	-48	33	-12	3.5388
MCI	Widespread bilateral posterior cingulate, medial and lateral parietal, temporal, occipital, basal ganglia, thalamus	4131	0	-54	27	53.8787
	Widespread bilateral medial frontal, anterior cingulate	2426	3	54	12	10.1883
	L middle temporal	216	-66	-12	-18	7.9563
	R middle temporal	142	63	-3	-24	7.4053
	R cerebellum	41	9	-54	-45	6.5141
	L cerebellum	29	-9	-57	-45	6.4655
	L cerebellum	48	-30	-81	-33	5.1676
	R parahippocampal	5	27	-33	-18	4.6878
	R cerebellum	36	42	-69	-39	4.5733
	R superior temporal	17	45	21	-33	4.5437
	R cerebellum	74	30	-84	-30	4.3973
	R thalamus	5	9	-12	9	4.3221
	L cerebellum	15	-42	-63	-48	4.2190
	L brainstem	9	-3	-30	-6	4.1668
	L caudate	8	-15	18	-3	4.1087
	R middle temporal	20	63	-33	-9	3.9644
	R anterior cingulate	9	3	18	18	3.8263
	R middle temporal	9	63	-24	-18	3.7045

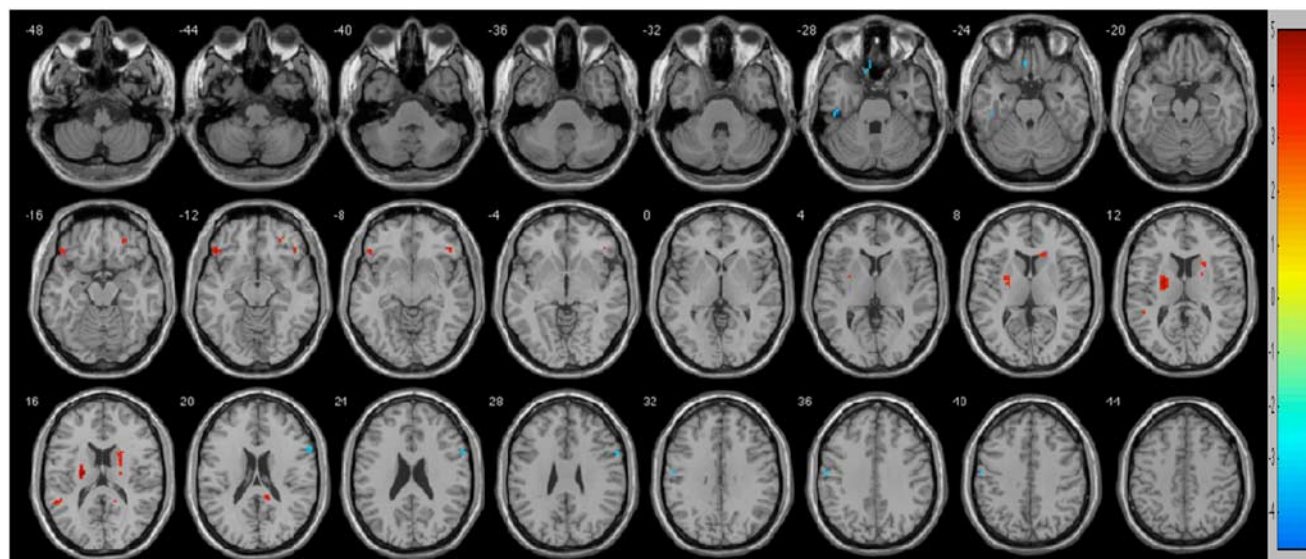
Seed ROI MNI coordinates:  $x = 0$ ,  $y = -53$ ,  $z = 26$ ; radius = 4 mm;  $p < 0.001$ , cluster size  $> 5$  voxels, false-discovery rate (FDR) corrected at  $p < .01$ .

inversely with the right caudate and directly with the left superior temporal region at the  $p < .05$  level. Processing speed domain z-scores correlated directly with the right inferior frontal region at the  $p < .05$  level.

## DISCUSSION

This study examined functional connectivity in the Default Mode Network in a well-characterized sample of older persons with and without mild cognitive impairment. A different pattern

of functional connectivity between the posterior cingulate and specific brain regions was observed between the two groups after adjusting for potential confounding variables. Specifically, there was less functional connectivity between the posterior cingulate cortex and the left and right orbital frontal, right middle frontal, left putamen, right caudate, left superior temporal, and right posterior cingulate regions in persons with MCI. There was also greater functional connectivity between the posterior cingulate cortex and right inferior frontal, left fusiform, left rectal, and left precentral regions in



**Fig. 2.** Regions of contrast between participants with no cognitive impairment (NCI) and mild cognitive impairment (MCI). Regions of greater connectivity for the NCIs are in red. Regions of greater connectivity for the MCIs are in blues. To control for multiple comparisons and spurious findings, we used the following consistent with our false discovery rate corrected within group analyses:  $p < .001$ , cluster size  $> 5$  voxels.

**Table 3.** Results of voxel-wise, between-group contrasts of z-transformed functional connectivity values (MCI versus NCI) while accounting for the effects of total gray matter volume

Location of Maximum Intensity Voxel	# Voxels	MNI Coordinates			<i>t</i> -value
<b>NCI &gt; MCI</b>					
L orbital frontal	13	-48	30	-12	4.2153
R orbital frontal	8	45	30	-12	3.9043
R middle frontal	5	24	42	-15	3.8609
L putamen	52	-24	-6	12	4.9792
R caudate 1	7	18	27	6	4.1524
R caudate 2	22	21	-12	18	4.0735
L superior temporal	10	-54	-48	15	3.9342
R posterior cingulate	13	12	-42	18	4.7002
<b>MCI &gt; NCI</b>					
L fusiform	5	-45	-27	-27	4.6011
L rectal	7	-6	30	-27	3.9158
R inferior frontal	12	60	12	24	3.8467
L precentral	6	-57	-9	36	4.1251

To control for multiple comparisons and spurious findings, we used the following consistent with our within-group false discovery rate threshold:  $p < .001$ , cluster size  $> 5$  voxels.

persons with MCI. Furthermore, functional connectivity values in the right caudate, left superior temporal, and right inferior frontal regions correlated with measures of cognition after adjusting for the effects of age, education, and gender.

An association between the Default Mode Network, amyloid burden, and episodic memory has been previously demonstrated (Buckner et al., 2005). In addition, recent evidence (Wang et al., 2010) suggests that functional connectivity of the posteriomedial cortices and the temporal lobe may be associated with memory performance on cognitive tasks. Our results are consistent with these findings and

extend them to other brain regions and another domain of cognition beyond episodic memory.

A central finding of the present study is that reduced functional connectivity in the striatum was observed in MCI. This is particularly noteworthy in that striatal structures are not typically considered part of the Default Mode Network. Although the striatum have previously received relatively little attention as key brain structures in cognitive aging and the development and progression of Alzheimer's disease, it is known that amyloid deposition occurs in the striatum in AD (Braak & Braak, 1990; Klunk et al., 2004), reduced putamen volume is associated with global cognitive performance in AD (De Jong et al., 2008), and recent work using  $^{11}\text{C}$ -labeled Pittsburgh Compound B (Koivunen et al., 2011) and novel anatomical connectivity mapping approaches (Bozzali et al., 2011) have implicated striatal structures as particularly sensitive to AD progression. Generally speaking, striatal caudate and putamen structures have robust connections with anterior and posterior cortices, and functional connectivity changes in these structures may be a reasonable indicator for significant intrinsic network alterations secondary to AD pathological changes. The striatum has projections to the prefrontal cortex, the primary and supplementary motor area, the primary somatosensory area, the premotor area, the temporal lobes, the occipital lobes, the cerebellum, and the thalamus, making the striatum a set of structures that may be sensitive to functional changes in multiple brain regions. It is difficult, however, to determine if functional connectivity differences in the striatum are due to primary changes in the function of the striatum or secondary changes in the regions associated with the striatum through their projections. More work is needed to clarify the role of the functional connectivity of the striatum in cognitive aging and AD.

Greater functional connectivity of the right inferior frontal region with the posterior cingulate cortex was observed among

**Table 4.** Statistics for demographic and cognitive variables for the non-cognitive impaired alternate sample of participants (N = 113)

	Alternate sample n = 113
Age (years)	
Mean (SD)	79.67 (7.09)
Range	60–93
Education (years)	
Mean (SD)	15.34 (3.15)
Range	8–28
MMSE (total score)	
Mean (SD)	28.89 (1.18)
Range	25–30
Sex	
% Female	77.6 (n = 90)
Race	
% White	94.8 (n = 110)
Global Cognition (z-score)	0.44 (0.43)
Episodic Memory (z-score)	0.56 (0.51)
Semantic Memory (z-score)	0.45 (0.51)
Working Memory (z-score)	0.31 (0.65)
Processing Speed (z-score)	0.36 (0.69)
Perceptual Organization (z-score)	0.39 (0.62)

Data are summarized as mean (standard deviation = *SD*) or as number (%). Age and education are presented in years; MMSE is total score; global cognition, episodic memory, semantic memory, working memory, processing speed, and perceptual organization are presented as z-scores.

MCI participants, and functional connectivity values were directly correlated with measures of processing speed in the alternate non-cognitively impaired group. Strengthening of the functional connectivity of the posterior cingulate cortex and right frontal regions is consistent with the findings of another resting-state functional connectivity study in MCI (Bai et al., 2009) and with the hypothesis that right frontal regions may serve a compensatory response among those at risk for AD (Han et al., 2007). Longitudinal studies are needed to determine if functional connectivity changes between the posterior cingulate cortex and the right inferior frontal region are associated with development of MCI and subsequent AD.

In this study, posterior cingulate cortex functional connectivity differences correlated with scores in the cognitive domains of episodic memory and processing speed. To date, the relation between functional connectivity of the posterior cingulate cortex and performance in cognitive domains has been somewhat unclear. While functional connectivity of the posterior cingulate cortex and associated structures has been associated with other cognitive abilities such as processing speed and attention in studies with relatively low participant numbers (e.g., Bai et al., 2009; Sorg et al., 2007), our findings indicate that functional connectivity of these structures may have particular significance for episodic memory and processing speed in the context of MCI and may reflect the presence of widespread AD pathology and an impending diagnosis of clinical AD. Furthermore, it was noted that functional connectivity increases in the striatum and decreases in the superior temporal region correlated with episodic memory

**Table 5.** Partial correlations between cognitive abilities and levels of connectivity in regions of interest after controlling for age, education, and sex in the alternate sample (N = 113) of non-cognitively impaired older adults.

	Alternate sample partial correlations											
	L Orbital Frontal	R Orbital Frontal	R Middle Frontal	L Putamen	R Caudate 1	R Caudate 2	L Superior Temporal	R Posterior Cingulate	L Fusiform	L Rectal	R Inferior Frontal	L Precentral
Episodic Memory	0.044	0.068	0.076	0.141	-0.220*	0.052	0.202*	0.077	-0.032	0.057	0.026	-0.025
Semantic Memory	-0.200	0.000	0.084	0.101	0.031	0.091	-0.001	-0.031	0.125	0.092	-0.017	0.013
Working Memory	-0.027	0.009	-0.039	-0.017	-0.082	-0.023	0.009	-0.123	0.056	0.032	0.101	-0.024
Processing Speed	0.013	0.058	0.016	0.040	0.036	-0.037	0.081	-0.056	-0.056	0.108	0.206*	0.162
Perceptual Organization	0.105	-0.012	-0.078	-0.102	-0.029	-0.044	0.065	0.029	-0.138	0.165	0.088	-0.005
Global Cognition	-0.007	0.051	0.032	0.077	-0.111	0.017	0.135	-0.020	-0.015	0.116	0.123	0.040

Two-tailed Pearson *r* values presented. Note. Coordinates are presented in MNI space. \**p* < .05.



performance. This functional connectivity direction difference highlights another contribution of the present study, that cognitive changes may be associated with co-occurring increases and decreases in functional connectivity of specific brain regions.

Limitations of this study include the restriction of the seed region to the posterior cingulate cortex. However, the posterior cingulate cortex has been established as a reliable seed region of interest for establishing the functional connectivity of the Default Mode Network (Greicius et al., 2003; Bai et al., 2009), and the reliability of other seed regions is less known. Even so, it is possible that seeding regions other than the posterior cingulate cortex may reveal a different pattern of functional connectivity between persons with and without MCI. Another limitation is that the analysis of the association between cognitive performance and connectivity levels in regions with significant group differences in functional connectivity was not controlled for multiple comparisons. Controlling for multiple comparisons yielded no significant correlations. These results are thus exploratory but nonetheless we believe they have important clinical implications. An additional limitation is the lack of inclusion of another set of MCI participants in our alternate sample for our cognitive measure partial correlation analyses. Our alternate sample is not reflective of the combined sample's characteristics since it is a non-cognitively impaired sample; however, we viewed this as a conservative approach to protect against the threat of multicollinearity and circularity of findings since our MCI and non-cognitive impaired groups were already distinguished based on cognitive measures. The lack of racial diversity of our sample yields another significant limitation as the present results may not be generalizable to members of other racial backgrounds. A final limitation is the study design is cross-sectional. However, the participants are followed annually and we will have the opportunity to examine the association between functional connectivity patterns and transition to MCI and AD in future analyses.

Strengths of this study include the use of a large community-based sample, examination of the relation between multiple cognitive domains and resting-state functional connectivity values, and control of factors known to influence cognition and resting-state functional connectivity values: age, education, sex, and total gray matter volume. Future research is needed to establish the time course relationship between changes in functional connectivity and cognitive performance; it is not known whether changes in functional connectivity precede a change in cognition or vice versa. Regardless of directionality, resting-state functional imaging has strong potential to become a widely used community-based neuroimaging biomarker for identifying persons at risk of developing AD, particularly when used in combination with other established biomarkers for the disease.

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